

## Feasibility of High Frame Rate 3-D Intracardiac Echography using Fan-Beam Transmissions

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## Feasibility of High Frame Rate 3-D Intracardiac Echography using Fan-Beam Transmissions

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### Background, Motivation and Objective

Intracardiac echography (ICE) is widely exploited for RF ablation procedures to guide the electrophysiologist in navigating the ablation catheter. High frame rate (HFR) 3D ICE could provide 3D imaging of electromechanical wave propagation (EWI) with higher spatiotemporal resolution than conventional methods. Yet, 3D probes generally make trade-offs among channel count, image quality, and frame rate. In this work, we propose a 1D micro beamforming (MBF) approach in elevation (El) direction to reduce the channel count while maintaining a HFR and image quality comparable to a fully sampled acquisition (FSA).

### Statement of Contribution/Methods

MBF is a well-established method to reduce the channel count while preserving the image quality and SNR for volumetric imaging. Generally, to suppress grating lobes and clutter, many narrow steered beams are transmitted. To achieve HFR for 3-D EWI ( $>1000\text{Hz}$ ), the number of transmissions should be kept below 7 per volume. We propose a 1D MBF with narrow beams in El and a diverging wave in azimuth (Az) direction. We transmit a beam profile of  $90^\circ \times 25^\circ$ , steered from  $-30^\circ$  to  $30^\circ$ , in steps of  $10^\circ$ . Transducer aperture is  $12.5 \times 3\text{mm}$  (Az $\times$ El), consisting of  $100 \times 24$  square elements, with a pitch of  $125\mu\text{m}$  ( $7.5\text{MHz}$ ). The final 3D image is formed by angle-weighted averaging of the sub-volumes reconstructed by voxel-based delay and sum per transmission. Image quality for different MBF sizes is compared to FSA based on lateral resolution, side-lobe levels, and contrast to noise ratio (CNR) in FIELD II simulations.

### Results/Discussion

The combination of diverging wave in Az and narrow beam in El with MBF size of 3-6 elements can provide HFR 3D imaging with an acceptable image quality and a corresponding channel count reduction (Fig 1). The image quality degraded for larger MBF sizes. The lateral resolution was 4.6mm and 1mm (same as FSA) at 50mm depth for El and Az direction respectively. The side-lobe levels and CNR in Az was -15dB and 2.2 respectively.

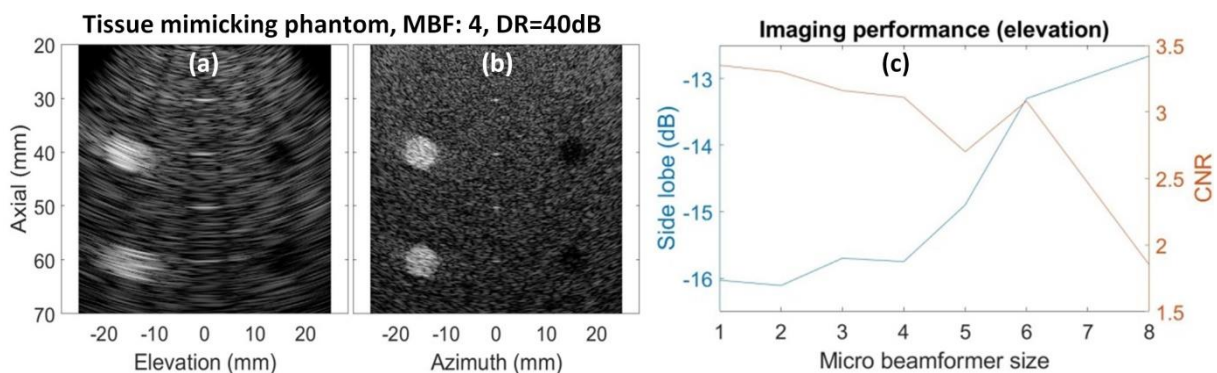


Figure 1.a) A 3D simulated tissue mimicking phantom imaged by the proposed method in elevation and b) in azimuth direction. c) side lobe level and contrast to noise ratio vs. MBF size in elevation