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DOI

[10.1109/TAP.2021.3111324](https://doi.org/10.1109/TAP.2021.3111324)

Publication date

2022

Document Version

Final published version

Published in

IEEE Transactions on Antennas and Propagation

Citation (APA)

Fuchs, P. S., & Remis, R. F. (2022). Generalized Signal Models and Direct FID-Based Dielectric Parameter Retrieval in MRI. *IEEE Transactions on Antennas and Propagation*, 70(2), 1451-1461. Article 9539065. <https://doi.org/10.1109/TAP.2021.3111324>

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Generalized Signal Models and Direct FID-Based Dielectric Parameter Retrieval in MRI

Patrick S. Fuchs¹, *Student Member, IEEE*, and Rob F. Remis¹

Abstract—In this article, we present full-wave signal models for magnetic and electric field measurements in magnetic resonance imaging (MRI). Our analysis is based on a scattering formalism in which the presence of an object or body is taken into account via an electric scattering source. We show that these signal models can be evaluated, provided that Green's tensors of the background field are known along with the dielectric parameters of the object and the magnetization within the excited part of the object. Furthermore, explicit signal expressions are derived in the case of a small homogeneous ball that is embedded in free space and for which the quasi-static Born approximation can be applied. The conductivity and permittivity of the ball appear as explicit parameters in the resulting signal models and allow us to study the sensitivity of the measured signals with respect to these dielectric parameters. Moreover, for free induction decay signals, we show through simulations that, under certain conditions, it is possible to retrieve the dielectric parameters of the ball from noise-contaminated induction decay signals that are based on electric or magnetic field measurements.

Index Terms—Born approximation, dielectric parameter retrieval, free induction decay (FID), magnetic resonance imaging (MRI), scattering formalism.

I. INTRODUCTION

THE influence of biological tissue on a typical magnetic resonance imaging (MRI) experiment (and previously in nuclear magnetic resonance (NMR) or zeugmatography [1]) has been investigated almost as long as the imaging modality exists. Most of this research has focused on the signal-to-noise ratio (SNR) of the received signals [2] and on the influence of tissue on the antenna sensitivity patterns [3]. Both of these aspects play an important role in understanding the structure of the received signal, of course, and are taken into account in signal optimization frameworks as shown in the recent work [4], for example. However, the influence of scattering currents induced in biological tissue through the magnetization itself is neglected in research on this matter up till now.

Due to the relationship between the SNR and the MRI background field, there is a continuing push to higher field strengths to achieve improved SNRs and faster scan times. These improvements do come at a cost as with higher field strengths also the frequency at which the MRI measurement

is performed increases. This higher frequency leads to new challenges in RF coil design, for example, and the received signals are generally more sensitive to changes in the dielectric (tissue) parameters as well.

In RF coil design, a major challenge at higher fields is to achieve a uniform excitation of the region of interest (ROI). Since the size of the object is on the order of the wavelength, nonuniform RF fields and interference patterns may appear within the ROI. Possible solutions are increasing antenna array sizes and combining antenna types although it has been demonstrated that such an approach has diminishing returns for larger array sizes [5]. Another approach is varying the array elements, using dipoles [6], combining loops and dipoles [7], [8], or using “special” fractionated dipoles [9]. In most of these approaches, the goal is to optimize the so-called ultimate intrinsic SNR (UISNR) or, in other words, to approximate ideal current patterns, which would lead to the highest SNR [4]. Originally, the term UISNR was introduced in [10] but additions have been made ever since, covering parallel MRI [11], current patterns required to attain this ratio [4], and addition of the specific absorption rate (SAR) [12].

For the SAR, all the abovementioned challenges are combined, as the higher heterogeneity of the RF fields leads to a local increase in tissue heating, which limits the amount of current that can be used to power measurement and, thus, limits the SNR that can be obtained for specific field strength and antenna array. Validated simulation techniques may be used to obtain more accurate local SAR estimates and may lead to antenna designs with reduced restrictions on the antenna currents that can be employed, or dielectric pads (passive shimming) can be used to improve the field homogeneity and reduce local heating effects [13].

In this article, we focus on the signal modeling part and derive full-wave signal models based on Maxwell's equations. Electric and magnetic field measurements are considered, and we show that the resulting signals are due to the time-varying magnetization inside the object and the induced electric scattering currents, each weighted by their own receive field as determined by the coil or antenna that is used for reception. The signal models can be explicitly evaluated provided Green's tensors of the background medium and the medium parameters of the object are known. Moreover, to gain further insight into how the electromagnetic medium parameters of the object influence the measured signal, explicit time- and frequency-domain signal models are derived for a special case, where the background medium consists of air and the object is a homogeneous ball that is uniformly excited and for which the Born approximation applies. Quasi-static signal

Manuscript received March 11, 2020; revised June 23, 2021; accepted August 6, 2021. Date of publication September 15, 2021; date of current version February 3, 2022. (*Corresponding author: Patrick S. Fuchs.*)

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Color versions of one or more figures in this article are available at <https://doi.org/10.1109/TAP.2021.3111324>.

Digital Object Identifier 10.1109/TAP.2021.3111324

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representations are derived from the full-wave signal models, and through a series of numerical experiments, we verify our models for the received signals. Finally, we demonstrate that, under certain conditions, it is possible to retrieve the dielectric parameters of the ball from measured free induction decay (FID) signals that are based on electric or magnetic field measurements. Electromagnetic field simulations are presented in which we validate our approach.

We present our analysis in the Laplace- or s -domain since it allows us to easily obtain frequency-domain solutions by letting $s \rightarrow j\omega$ via the right-half of the complex s -plane or time-domain field responses using standard Laplace transformation rules.

II. THEORY

Let \mathbb{D}_{obj} be a bounded domain occupied by a penetrable object that is present in an MR scanner. We assume that the complete object or part of this object has been excited during the transmit state of the scanner. More precisely, we assume that the temporal derivative of magnetization $\partial_t \mathbf{M}(\mathbf{x}, t)$ is nonzero within the subdomain $\mathbb{D}_{\text{ex}} \subseteq \mathbb{D}_{\text{obj}}$ and vanishes outside this domain. In other words, $\partial_t \mathbf{M}(\mathbf{x}, t)$ has the domain \mathbb{D}_{ex} as its spatial support and $\mathbb{D}_{\text{ex}} = \mathbb{D}_{\text{obj}}$ if the complete object is excited.

Measurements are carried out outside the object and take place in free space. To set up the data models that describe our measurements, we first consider a surface S with unit normal \mathbf{v} and closed boundary curve C with a unit normal $\boldsymbol{\tau}$ along this curve such that $\boldsymbol{\tau}$ and \mathbf{v} are oriented according to the right-hand rule. The surface S has an area A , and the position vector of its barycenter is denoted by \mathbf{x}_R . The surface is completely located in air and is used to measure the electromotive or magnetomotive force given by

$$\hat{V}_{\text{emf}}(s) = \int_{\mathbf{x} \in C} \hat{\mathbf{E}} \cdot \boldsymbol{\tau} d\ell \quad \text{and} \quad \hat{I}_{\text{mmf}}(s) = \int_{\mathbf{x} \in C} \hat{\mathbf{H}} \cdot \boldsymbol{\tau} d\ell \quad (1)$$

respectively. Using Maxwell's equations and assuming that the area A of the surface is sufficiently small (diameter much smaller than the smallest wavelength of interest), we have

$$\hat{V}_{\text{emf}}(s) = -s \int_{\mathbf{x} \in S} \hat{\mathbf{B}} \cdot \mathbf{v} dA \approx -s \mu_0 A \hat{\mathbf{H}}(\mathbf{x}_R, s) \cdot \mathbf{v} \quad (2)$$

where we have used $\hat{\mathbf{B}} = \mu_0 \hat{\mathbf{H}}$ since the measurement surface S is located in air. Similarly, for the magnetomotive force, we obtain

$$\hat{I}_{\text{mmf}}(s) = s \int_{\mathbf{x} \in S} \hat{\mathbf{D}} \cdot \mathbf{v} dA \approx s \varepsilon_0 A \hat{\mathbf{E}}(\mathbf{x}_R, s) \cdot \mathbf{v} \quad (3)$$

where we have used $\hat{\mathbf{D}} = \varepsilon_0 \hat{\mathbf{E}}$. Assuming that a measurement is linear and time-invariant, we can generalize our field measurement description to

$$\hat{d}_h(s) = \int_{\mathbf{x} \in \mathbb{D}_{\text{rec}}} \hat{\mathbf{m}}_h(\mathbf{x}, s) \cdot \hat{\mathbf{H}}(\mathbf{x}, s) dV \quad (4)$$

and

$$\hat{d}_e(s) = \int_{\mathbf{x} \in \mathbb{D}_{\text{rec}}} \hat{\mathbf{m}}_e(\mathbf{x}, s) \cdot \hat{\mathbf{E}}(\mathbf{x}, s) dV \quad (5)$$

in which a volumetric receiver is used to obtain the measured signals. The receiver is completely located outside the object and occupies the receiver domain \mathbb{D}_{rec} , and its action on the electromagnetic field inside the receiver domain is described by the vectorial receiver functions $\hat{\mathbf{m}}_h$ and $\hat{\mathbf{m}}_e$ for magnetic and electric field measurements, respectively. Note that the electromotive and magnetomotive forces are special cases of (4) and (5). In particular, with

$$\hat{\mathbf{m}}_h(s) = s \mu_0 A \delta(\mathbf{x} - \mathbf{x}_R) \mathbf{v} \quad (6)$$

and

$$\hat{\mathbf{m}}_e(s) = s \varepsilon_0 A \delta(\mathbf{x} - \mathbf{x}_R) \mathbf{v} \quad (7)$$

we have $\hat{d}_h(s) = -\hat{V}_{\text{emf}}(s)$ and $\hat{d}_e(s) = \hat{I}_{\text{mmf}}(s)$. Since an electromotive force measurement is characterized by (4) and (6), these equations provide a model for a magnetic field measurement. Similarly, a magnetomotive force measurement is characterized by (5) and (7), and these equations provide a model for an electric field measurement. In the following, we take the general signal models (4) and (5) as a starting point and consider the electromotive and magnetomotive forces as special cases.

A. Scattering Formalism

To further develop the signal models (4) and (5), the magnetic and electric field strengths inside the receiver domain are obviously required. To this end, we set up a scattering formalism and write the electromagnetic field as a superposition of a background and a scattered field. The background field is defined as the field that is present when the constitutive parameters within the object domain are the same as the parameters of the background medium, while the scattered field takes the presence of the object into account. Assuming that the background can be accurately described by a background conductivity $\sigma_b(\mathbf{x})$, a background permittivity $\varepsilon_b(\mathbf{x})$, and a permeability $\mu_b(\mathbf{x})$, the Laplace-domain background field satisfies Maxwell's equations

$$-\nabla \times \hat{\mathbf{H}}^b + \sigma_b \hat{\mathbf{E}}^b + s \varepsilon_b \hat{\mathbf{E}}^b = \mathbf{0} \quad (8)$$

and

$$\nabla \times \hat{\mathbf{E}}^b + s \mu_b \hat{\mathbf{H}}^b = -\hat{\mathbf{K}} \quad (9)$$

where $\hat{\mathbf{K}}$ is the Laplace transform of $\mu_0 \partial_t \mathbf{M}$ with $\mathbf{M}(\mathbf{x}, t)$ being the time-varying magnetization with the domain \mathbb{D}_{ex} as its spatial support. Across interfaces where the background medium parameters exhibit a jump, the above Maxwell's equations have to be supplemented by the appropriate boundary conditions, and if perfectly conducting structures are present in the background configuration, then the boundary condition for a perfectly conducting structure has to be included as well, of course. For general inhomogeneous background configurations that can be described in terms of the background medium parameters, the above Maxwell's equations can only be solved numerically. Formally, however, we can express the electromagnetic background field in terms of Green's tensors of the background medium as

$$\hat{\mathbf{H}}^b(\mathbf{x}, s) = \int_{\mathbf{x}' \in \mathbb{D}_{\text{ex}}} \hat{\mathbf{G}}^{\text{HK}}(\mathbf{x}, \mathbf{x}', s) \cdot \hat{\mathbf{K}}(\mathbf{x}', s) dV \quad (10)$$

and

$$\hat{\mathbf{E}}^b(\mathbf{x}, s) = \int_{\mathbf{x}' \in \mathbb{D}_{\text{ex}}} \hat{\mathbf{G}}^{\text{EK}}(\mathbf{x}, \mathbf{x}', s) \cdot \hat{\mathbf{K}}(\mathbf{x}', s) dV \quad (11)$$

where $\hat{\mathbf{G}}^{\text{HK}}$ and $\hat{\mathbf{G}}^{\text{EK}}$ are the magnetic current to magnetic field and the magnetic current to electric field Green's tensors of the background medium.

Furthermore, the scattered field $\{\hat{\mathbf{H}}^{\text{sc}}, \hat{\mathbf{E}}^{\text{sc}}\}$ satisfies Maxwell's equations

$$-\nabla \times \hat{\mathbf{H}}^{\text{sc}} + \sigma_b \hat{\mathbf{E}}^{\text{sc}} + s \varepsilon_b \hat{\mathbf{E}}^{\text{sc}} = -\hat{\mathbf{J}}^{\text{sc}} \quad (12)$$

and

$$\nabla \times \hat{\mathbf{E}}^{\text{sc}} + s \mu_b \hat{\mathbf{H}}^{\text{sc}} = \mathbf{0} \quad (13)$$

where $\hat{\mathbf{J}}^{\text{sc}}$ is the Laplace transformed dielectric scattering source given by

$$\hat{\mathbf{J}}^{\text{sc}}(\mathbf{x}, s) = \{\hat{\sigma}(\mathbf{x}) - \sigma_b(\mathbf{x}) + s[\hat{\varepsilon}(\mathbf{x}) - \varepsilon_b(\mathbf{x})]\} \hat{\mathbf{E}}(\mathbf{x}, s) \quad (14)$$

for $\mathbf{x} \in \mathbb{D}_{\text{obj}}$, where $\hat{\sigma}(\mathbf{x})$ is the conductivity of the object and $\hat{\varepsilon}(\mathbf{x})$ is its permittivity. The object is assumed to have no contrast in its permeability with respect to the background medium.

For the scattered field, we have the integral representations

$$\hat{\mathbf{H}}^{\text{sc}}(\mathbf{x}, s) = \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \hat{\mathbf{G}}^{\text{HJ}}(\mathbf{x}, \mathbf{x}', s) \cdot \hat{\mathbf{J}}^{\text{sc}}(\mathbf{x}', s) dV \quad (15)$$

and

$$\hat{\mathbf{E}}^{\text{sc}}(\mathbf{x}, s) = \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \hat{\mathbf{G}}^{\text{EJ}}(\mathbf{x}, \mathbf{x}', s) \cdot \hat{\mathbf{J}}^{\text{sc}}(\mathbf{x}', s) dV \quad (16)$$

where $\hat{\mathbf{G}}^{\text{HJ}}$ and $\hat{\mathbf{G}}^{\text{EJ}}$ are the electric current to magnetic field and the electric current to electric field Green's tensors of the background medium. Having the integral representations for the background and scattered fields at our disposal, we can now further develop the full-wave signal models (4) and (5).

B. Full-Wave Signal Model

Writing the total magnetic and electric fields in the receiver domain as a superposition of the background and scattered fields and using the integral representations (10), (11), (15), and (16), the signal models of (4) and (5) become

$$\begin{aligned} \hat{d}_h(s) &= \int_{\mathbf{x} \in \mathbb{D}_{\text{ant}}} \hat{\mathbf{m}}_h(\mathbf{x}, s) \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{ex}}} \hat{\mathbf{G}}^{\text{HK}}(\mathbf{x}, \mathbf{x}', s) \cdot \hat{\mathbf{K}}(\mathbf{x}', s) dV dV \\ &\quad + \int_{\mathbf{x} \in \mathbb{D}_{\text{ant}}} \hat{\mathbf{m}}_h(\mathbf{x}, s) \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \hat{\mathbf{G}}^{\text{HJ}}(\mathbf{x}, \mathbf{x}', s) \cdot \hat{\mathbf{J}}^{\text{sc}}(\mathbf{x}', s) dV dV \end{aligned} \quad (17)$$

and

$$\begin{aligned} \hat{d}_e(s) &= \int_{\mathbf{x} \in \mathbb{D}_{\text{ant}}} \hat{\mathbf{m}}_e(\mathbf{x}, s) \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{ex}}} \hat{\mathbf{G}}^{\text{EK}}(\mathbf{x}, \mathbf{x}', s) \cdot \hat{\mathbf{K}}(\mathbf{x}', s) dV dV \\ &\quad + \int_{\mathbf{x} \in \mathbb{D}_{\text{ant}}} \hat{\mathbf{m}}_e(\mathbf{x}, s) \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \hat{\mathbf{G}}^{\text{EJ}}(\mathbf{x}, \mathbf{x}', s) \cdot \hat{\mathbf{J}}^{\text{sc}}(\mathbf{x}', s) dV dV. \end{aligned} \quad (18)$$

Interchanging the order of integration and using the reciprocity properties of Green's tensors [14] allow us to write the signal representations as

$$\begin{aligned} \hat{d}_h(s) &= \int_{\mathbf{x}' \in \mathbb{D}_{\text{ex}}} \hat{\mathbf{K}}(\mathbf{x}', s) \cdot \hat{\mathbf{W}}_h^{\text{mg}}(\mathbf{x}', s) dV \\ &\quad - \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \hat{\mathbf{J}}^{\text{sc}}(\mathbf{x}', s) \cdot \hat{\mathbf{W}}_e^{\text{mg}}(\mathbf{x}', s) dV \end{aligned} \quad (19)$$

and

$$\begin{aligned} \hat{d}_e(s) &= - \int_{\mathbf{x}' \in \mathbb{D}_{\text{ex}}} \hat{\mathbf{K}}(\mathbf{x}', s) \cdot \hat{\mathbf{W}}_h^{\text{el}}(\mathbf{x}', s) dV \\ &\quad + \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \hat{\mathbf{J}}^{\text{sc}}(\mathbf{x}', s) \cdot \hat{\mathbf{W}}_e^{\text{el}}(\mathbf{x}', s) dV \end{aligned} \quad (20)$$

where we have introduced the receive fields for a magnetic field measurement as

$$\hat{\mathbf{W}}_h^{\text{mg}}(\mathbf{x}', s) = \int_{\mathbf{x} \in \mathbb{D}_{\text{rec}}} \hat{\mathbf{G}}^{\text{HK}}(\mathbf{x}', \mathbf{x}, s) \cdot \hat{\mathbf{m}}_h(\mathbf{x}, s) dV \quad (21)$$

and

$$\hat{\mathbf{W}}_e^{\text{mg}}(\mathbf{x}', s) = \int_{\mathbf{x} \in \mathbb{D}_{\text{rec}}} \hat{\mathbf{G}}^{\text{EK}}(\mathbf{x}', \mathbf{x}, s) \cdot \hat{\mathbf{m}}_h(\mathbf{x}, s) dV \quad (22)$$

while the receive fields for an electric field measurement are given by

$$\hat{\mathbf{W}}_h^{\text{el}}(\mathbf{x}', s) = \int_{\mathbf{x} \in \mathbb{D}_{\text{rec}}} \hat{\mathbf{G}}^{\text{HJ}}(\mathbf{x}', \mathbf{x}, s) \cdot \hat{\mathbf{m}}_e(\mathbf{x}, s) dV \quad (23)$$

and

$$\hat{\mathbf{W}}_e^{\text{el}}(\mathbf{x}', s) = \int_{\mathbf{x} \in \mathbb{D}_{\text{rec}}} \hat{\mathbf{G}}^{\text{EJ}}(\mathbf{x}', \mathbf{x}, s) \cdot \hat{\mathbf{m}}_e(\mathbf{x}, s) dV. \quad (24)$$

Equations (19) and (20) are the full-wave signal models for magnetic and electric field measurements, respectively, in which the magnetic-current source (magnetization) and the scattering source contribute to the measured signal both weighted by their respective antenna receive fields. These receive fields depend on Green's tensors of the background medium and the coils or antennas used for reception and clearly provide us with a means to optimize the received signal. In particular, in high-field MRI so-called signals voids are often observed in the resulting image, which is due to wave interference effects that take place within the body [15]. The impact of these interference effects on the received signal is captured by the second term on the right-hand sides of (19) and (20). Therefore, the above signal models can be used to minimize interference effects by designing receiving antennas or coils for which the corresponding magnetic receive fields $\hat{\mathbf{W}}_h^{\text{mg}}$ or $\hat{\mathbf{W}}_h^{\text{el}}$ are dominant and as uniform as possible. High permittivity pads [16] are also often used to eliminate signals voids in an MR image, and the above signal models can be used to optimize these pads and their location as well since their presence can be taken into account in the scattering current $\hat{\mathbf{J}}^{\text{sc}}(\mathbf{x}, s)$. In practice, the pads are placed in the neighborhood and on top of the body part that needs to be imaged. From the above signal models, it immediately follows that to have an effect on the received signal and ultimately an MR image; a pad should be placed at a location where the electric receive fields $\hat{\mathbf{W}}_e^{\text{mg}}$ and $\hat{\mathbf{W}}_e^{\text{el}}$ do not vanish. If this leads

to an unrealistic pad location, then different receive antennas or different receive locations (or both) must be used to image the desired field of view in which signal voids are eliminated or minimized.

Finally, in principle, the above signal models may also be used to retrieve the dielectric properties of the body part of interest. In this case, receiving antennas must be used for which the electric receive field $\hat{\mathbf{W}}_e^{\text{mg}}$ and $\hat{\mathbf{W}}_e^{\text{el}}$ are optimized, and the second terms on the right-hand sides of (19) and (20) are dominant. In fact, in Section III-C, we will show that, for the specific case of a homogeneous ball located in an air-filled background, this is essentially the case for an electric field dipole measurement but not for a magnetic field dipole measurement. In general, we have to resort to the signal models of (19) and (20), however, to design receive antennas or coils that are sensitive to the dielectric parameters of the object or body part of interest.

To evaluate these models, first, the magnetization (and, hence, the magnetic-current source $\hat{\mathbf{K}}$) must be known within the excited part \mathbb{D}_{ex} of the object since the time variations of this field quantity generate the radiated electromagnetic field. Second, the conductivity and permittivity profiles of the object must be known. This allows us to determine the electric field strength within the object by solving a forward problem with the magnetic-current density $\hat{\mathbf{K}}$ in \mathbb{D}_{ex} as a source. Finally, Green's tensors of the background medium must be known as well to determine the receive fields (21)–(24). In general, these tensors can only be determined through simulations since the background is inhomogeneous. In conclusion, the full-wave signals can be evaluated in principle, provided that: 1) the magnetization in \mathbb{D}_{ex} is known; 2) the conductivity and permittivity profiles of the object are known; and 3) Green's tensors of the background medium are known. Note that frequency-domain responses are obtained by letting $s \rightarrow j\omega$, and time-domain signal responses involve temporal convolutions of the magnetic-current source and the dielectric scattering source with their respective receive fields since their Laplace-domain counterparts all are s -dependent in general.

C. Simplified Full-Wave Signal Models for a Ball Located in Free-Space

Given the above observations, we consider a specific configuration for which it is possible to develop signal models that explicitly show how the received signals depend on the conductivity and permittivity of the object. In particular, we first consider a background medium consisting of free space. Green's tensors of the background medium and the receive fields for electromotive or magnetomotive force measurements (dipole measurements) can then be determined explicitly. Second, we take a small homogeneous ball with a constant conductivity σ and permittivity ε as our object of interest. Explicit signal models can then be developed, provided that the radius of the ball is sufficiently small.

Let the background medium be free space and consider an electromotive or magnetomotive force measurement. For an electromotive force measurement, the receive function $\hat{\mathbf{m}}_h$ is

given by (6), and since the background medium is free space, Green's tensors are explicitly known [14], and the receive fields follow as:

$$\begin{aligned}\hat{\mathbf{W}}_h^{\text{mg}}(\mathbf{x}', s) &= s\mu_0 A \hat{\mathbf{G}}^{\text{HK}}(\mathbf{x}', \mathbf{x}_R, s) \cdot \mathbf{v} \\ &= \frac{A}{4\pi |\mathbf{x}' - \mathbf{x}_R|^3} \exp(-s\tau) [(1 + s\tau)\mathbf{p}_1 + (s\tau)^2 \mathbf{p}_2]\end{aligned}\quad (25)$$

and

$$\begin{aligned}\hat{\mathbf{W}}_e^{\text{mg}}(\mathbf{x}', s) &= s\mu_0 A \hat{\mathbf{G}}^{\text{EK}}(\mathbf{x}', \mathbf{x}_R, s) \cdot \mathbf{v} \\ &= \frac{s\mu_0 A}{4\pi |\mathbf{x}' - \mathbf{x}_R|^2} \exp(-s\tau) (1 + s\tau) \mathbf{n} \times \mathbf{v}\end{aligned}\quad (26)$$

where $\tau = c_0^{-1} |\mathbf{x}' - \mathbf{x}_R|$ with c_0 being the electromagnetic wave speed in vacuum. It is clear that τ is the travel time from the point of integration \mathbf{x}' to the receiver location \mathbf{x}_R . Furthermore, $\mathbf{p}_1 = 3\mathbf{n}(\mathbf{n} \cdot \mathbf{v}) - \mathbf{v}$, and $\mathbf{p}_2 = \mathbf{n}(\mathbf{n} \cdot \mathbf{v}) - \mathbf{v}$ with $\mathbf{n} = (\mathbf{x}' - \mathbf{x}_R)/|\mathbf{x}' - \mathbf{x}_R|$ being the unit vector pointing from the receiver location to the point of integration.

Similarly, for a magnetomotive force measurement, the receive function $\hat{\mathbf{m}}_e$ is given by (7), and the receive fields follow as

$$\begin{aligned}\hat{\mathbf{W}}_h^{\text{el}}(\mathbf{x}, s) &= s\varepsilon_0 A \hat{\mathbf{G}}^{\text{HJ}}(\mathbf{x}, \mathbf{x}_R, s) \cdot \mathbf{v} \\ &= -\frac{s\varepsilon_0 A}{4\pi |\mathbf{x}' - \mathbf{x}_R|^2} \exp(-s\tau) (1 + s\tau) \mathbf{n} \times \mathbf{v}\end{aligned}\quad (27)$$

and

$$\begin{aligned}\hat{\mathbf{W}}_e^{\text{el}}(\mathbf{x}, s) &= s\varepsilon_0 A \hat{\mathbf{G}}^{\text{EJ}}(\mathbf{x}, \mathbf{x}_R, s) \cdot \mathbf{v} \\ &= \frac{A}{4\pi |\mathbf{x}' - \mathbf{x}_R|^3} \exp(-s\tau) [(1 + s\tau)\mathbf{p}_1 + (s\tau)^2 \mathbf{p}_2].\end{aligned}\quad (28)$$

Note that $\hat{\mathbf{W}}_e^{\text{mg}}$ and $\hat{\mathbf{W}}_h^{\text{el}}$ are proportional to each other, and $\hat{\mathbf{W}}_h^{\text{mg}} = \hat{\mathbf{W}}_e^{\text{el}}$.

Second, we take a small ball as our object of interest. The ball is centered at the origin of our reference frame and has a radius $a > 0$. It is characterized by a constant conductivity σ and permittivity ε , and its permeability is equal to that of free space. We assume that the radius a is so small that the ball is excited throughout ($\mathbb{D}_{\text{ex}} = \mathbb{D}_{\text{obj}}$), and time variations of the magnetization (and, hence, the magnetic-current source $\hat{\mathbf{K}}$) are uniform, that is, $\hat{\mathbf{K}}$ does not vary with position within the ball. For a given magnetization, the magnetic-current source is now known, and the total electric field within the ball can be computed by solving the integral equation

$$\begin{aligned}\hat{\mathbf{E}}(\mathbf{x}', s) &= \hat{\mathbf{E}}^{\text{b}}(\mathbf{x}', s) \\ &\quad - \hat{\chi}(\hat{\gamma}_0^2 - \nabla \cdot \nabla) \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \hat{\mathbf{G}}(\mathbf{x} - \mathbf{x}', s) \hat{\mathbf{E}}(\mathbf{x}', s) dV\end{aligned}\quad (29)$$

for the electric field $\hat{\mathbf{E}}(\mathbf{x}', s)$ with $\mathbf{x}' \in \mathbb{D}_{\text{obj}}$. In the above equation, $\hat{\gamma}_0 = s/c_0$ is the propagation coefficient of free space, $\hat{\chi} = \hat{\varepsilon}_r - 1 + \hat{\sigma}/(s\varepsilon_0)$ is the contrast of the ball, $\hat{\mathbf{G}}$ is the scalar Green's function of free space, and $\hat{\mathbf{E}}^{\text{b}}$ can be determined from (11) since $\hat{\mathbf{K}}$ is known. In Section III, we will essentially follow such an approach, except that we will

determine the electric field in the time-domain using FDTD for a given magnetization. Here, we use the above integral equation to arrive at the desired signal models. Specifically, let us consider frequencies of operation s and a ball of radius a with conductivity and permittivity values $\hat{\sigma}$ and $\hat{\epsilon}$, respectively, such that the condition

$$(2a|\hat{\gamma}_0|)^2|\hat{\chi}| \ll 1 \quad (30)$$

is satisfied. For 3-D scalar wave field problems, this is a sufficient condition for the Neumann series to converge [17], [18]. In addition, let us assume that there is (essentially) no charge accumulation at the boundary of the ball. The gradient-divergence term is then negligible, and the above integral equation turns into a scalar integral equation for each component of the electric field. Moreover, since we consider frequencies and dielectric parameters for which (30) holds, we may approximate

$$\hat{\mathbf{E}}(\mathbf{x}', s) \approx \hat{\mathbf{E}}^b(\mathbf{x}', s). \quad (31)$$

Now provided that the quasi-static condition $|2a\hat{\gamma}_0| \ll 1$ is also satisfied, this background field is essentially given by

$$\hat{\mathbf{E}}^b(\mathbf{x}', s) = -\frac{1}{3}\hat{\mathbf{K}} \times \mathbf{x}' \quad (32)$$

with $\mathbf{x}' \in \mathbb{D}_{\text{obj}}$. Notice that this background field does not have a radial component, which is consistent with our assumption of no charge accumulation at the boundary. Also, note that, if the quasi-static condition $|2a\hat{\gamma}_0| \ll 1$ holds, then (30) can be satisfied for $|\hat{\chi}| \gg 1$ [18].

Provided that the quasi-static and Born approximations hold, the dielectric scattering source within the ball is given by

$$\begin{aligned} \hat{\mathbf{J}}^{\text{sc}}(\mathbf{x}', s) &= [\hat{\sigma} + s(\hat{\epsilon} - \epsilon_0)]\hat{\mathbf{E}}(\mathbf{x}', s) \\ &= -\frac{1}{3}[\hat{\sigma} + s(\hat{\epsilon} - \epsilon_0)]\hat{\mathbf{K}}(s) \times \mathbf{x}' \end{aligned} \quad (33)$$

for $\mathbf{x}' \in \mathbb{D}_{\text{obj}}$. Substituting in (19) and (20), we obtain the signal models

$$\hat{d}_h(s) = \hat{\mathbf{K}}(s) \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \hat{\mathbf{S}}^{\text{mg}}(\mathbf{x}', s) dV \quad (34)$$

and

$$\hat{d}_e(s) = -\hat{\mathbf{K}}(s) \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \hat{\mathbf{S}}^{\text{el}}(\mathbf{x}', s) dV \quad (35)$$

where the vectorial sensitivity functions are given by

$$\hat{\mathbf{S}}^{\text{mg}}(\mathbf{x}', s) = \hat{\mathbf{W}}_h^{\text{mg}} + \hat{\chi}_e \mathbf{x}' \times \hat{\mathbf{W}}_e^{\text{mg}} \quad (36)$$

and

$$\hat{\mathbf{S}}^{\text{el}}(\mathbf{x}', s) = \hat{\mathbf{W}}_h^{\text{el}} + \hat{\chi}_e \mathbf{x}' \times \hat{\mathbf{W}}_e^{\text{el}} \quad (37)$$

with $\hat{\chi}_e = [\hat{\sigma} + s(\hat{\epsilon} - \epsilon_0)]/3 = s\epsilon_0\hat{\chi}/3$. Substituting expressions (25)–(28) for the receive fields in the above equations and assuming that the time derivative of the magnetization is band-limited and centered around the (Larmor) frequency ω_0 such that the conductivity and permittivity can be considered constant on this frequency band, we obtain by applying an inverse Laplace transform the time-domain signals

$$d_h(t) = \mu_0 \partial_t \mathbf{M}(t) \ast \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \mathbf{S}^{\text{mg}}(\mathbf{x}', t - \tau) dV \quad (38)$$

and

$$d_e(t) = -\mu_0 \partial_t \mathbf{M}(t) \ast \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \mathbf{S}^{\text{el}}(\mathbf{x}', t - \tau) dV \quad (39)$$

for $t > 0$, where the asterisk denotes convolution in time and the time-domain sensitivity functions are given by

$$\mathbf{S}^{\text{mg}}(\mathbf{x}', t) = \frac{A}{4\pi |\mathbf{x}' - \mathbf{x}_R|^3} \sum_{k=0}^3 \tau^k \delta^{(k)}(t) \mathbf{r}_k^{\text{mg}} \quad (40)$$

and

$$\mathbf{S}^{\text{el}}(\mathbf{x}', t) = \frac{A}{4\pi |\mathbf{x}' - \mathbf{x}_R|^3} \sum_{k=0}^3 \tau^k \delta^{(k)}(t) \mathbf{r}_k^{\text{el}} \quad (41)$$

where $\delta^{(k)}$ is the k th derivative of the Dirac distribution. Explicit expressions for the expansion vectors $\mathbf{r}_k^{\text{mg,el}}$, $k = 0, 1, 2, 3$, are given in the Appendix.

In the above signal models, propagation effects and travel times from the ball to the receiver are fully taken into account. However, when the receivers are located not too far from the ball (in a sense to be made precise), then the signals may be simplified even further. To this end, we substitute the receive fields of (25)–(28) into (36) and (37) and arrange the resulting expressions in such a way that the sensitivities are expanded in terms of vectors that do not depend on the distance $|\mathbf{x}' - \mathbf{x}_R|$. Carrying out these steps, we find for the magnetic field sensitivity function

$$\begin{aligned} \hat{\mathbf{S}}^{\text{mg}}(\mathbf{x}', s) &= \frac{A}{4\pi |\mathbf{x}' - \mathbf{x}_R|^3} \exp(-s\tau) \\ &\cdot [\mathbf{p}_1 + (s\tau)(\mathbf{p}_1 + \hat{\mathbf{q}}^{\text{mg}}) + (s\tau)^2(\mathbf{p}_2 + \hat{\mathbf{q}}^{\text{mg}})] \end{aligned} \quad (42)$$

while, for the sensitivity function for an electric field measurement, we have

$$\begin{aligned} \hat{\mathbf{S}}^{\text{el}}(\mathbf{x}', s) &= \frac{A}{4\pi |\mathbf{x}' - \mathbf{x}_R|^3} \exp(-s\tau) \\ &\cdot [\hat{\chi}_e \mathbf{x}' \times \mathbf{p}_1 \\ &\quad + (s\tau)(\hat{\chi}_e \mathbf{x}' \times \mathbf{p}_1 + Y_0 \mathbf{q}^{\text{el}}) \\ &\quad + (s\tau)^2(\hat{\chi}_e \mathbf{x}' \times \mathbf{p}_2 + Y_0 \mathbf{q}^{\text{el}})] \end{aligned} \quad (43)$$

with $\hat{\mathbf{q}}^{\text{mg}} = Z_0 \hat{\chi}_e [(\mathbf{x}' \cdot \mathbf{v})\mathbf{n} - (\mathbf{x}' \cdot \mathbf{n})\mathbf{v}]$ and $\mathbf{q}^{\text{el}} = \mathbf{v} \times \mathbf{n}$. Note that the vectors

$$\mathbf{p}_{1,2} + \hat{\mathbf{q}}^{\text{mg}} \quad \text{and} \quad \hat{\chi}_e \mathbf{x}' \times \mathbf{p}_{1,2} + Y_0 \mathbf{q}^{\text{el}} \quad (44)$$

are s -dependent but do not depend on $|\mathbf{x}' - \mathbf{x}_R|$. We can now use the above expressions to investigate which terms contribute to the received signals measured at different receiver locations. Specifically, let us first consider the case where we place the receiver near (almost at) the surface of the ball ($|\mathbf{x}_R| = a(1 + \epsilon)$, with $\epsilon > 0$ small). In this case, $|s\tau| \leq |\hat{\gamma}_0 2a| \ll 1$, and the receive field can be considered quasi-static. The signals

models simplify to

$$\begin{aligned} \hat{d}_h(s) &\approx \hat{d}_h^{QS}(s) \\ &= \frac{A}{4\pi} \left[\hat{\mathbf{K}} \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \frac{\mathbf{p}_1}{|\mathbf{x}' - \mathbf{x}_R|^3} dV \right. \\ &\quad \left. + s\mu_0 \hat{\chi}_e \hat{\mathbf{K}} \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \frac{(\mathbf{x}' \cdot \mathbf{v})\mathbf{n} - (\mathbf{x}' \cdot \mathbf{n})\mathbf{v}}{|\mathbf{x}' - \mathbf{x}_R|^2} dV \right] \end{aligned} \quad (45)$$

and

$$\begin{aligned} \hat{d}_e(s) &\approx \hat{d}_e^{QS}(s) \\ &= -\frac{A}{4\pi} \left[\hat{\chi}_e \hat{\mathbf{K}} \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \frac{\mathbf{x}' \times \mathbf{p}_1}{|\mathbf{x}' - \mathbf{x}_R|^3} dV \right. \\ &\quad \left. + s\varepsilon_0 \hat{\mathbf{K}} \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \frac{\mathbf{v} \times \mathbf{n}}{|\mathbf{x}' - \mathbf{x}_R|^2} dV \right] \end{aligned} \quad (46)$$

and their time-domain counterparts are given by

$$\begin{aligned} d_h^{QS}(t) &= \frac{\mu_0 A}{4\pi} \left[\partial_t \mathbf{M} \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \frac{\mathbf{p}_1}{|\mathbf{x}' - \mathbf{x}_R|^3} dV \right. \\ &\quad + \frac{\sigma \mu_0}{3} \partial_t^2 \mathbf{M} \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \frac{[(\mathbf{x}' \cdot \mathbf{v})\mathbf{n} - (\mathbf{x}' \cdot \mathbf{n})\mathbf{v}]}{|\mathbf{x}' - \mathbf{x}_R|^2} dV \\ &\quad \left. + \frac{\varepsilon_r - 1}{3} \frac{1}{c_0^2} \partial_t^3 \mathbf{M} \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \frac{[(\mathbf{x}' \cdot \mathbf{v})\mathbf{n} - (\mathbf{x}' \cdot \mathbf{n})\mathbf{v}]}{|\mathbf{x}' - \mathbf{x}_R|^2} dV \right] \end{aligned} \quad (47)$$

and

$$\begin{aligned} d_e^{QS}(t) &= -\frac{\mu_0 A}{4\pi} \left[\frac{\sigma}{3} \partial_t \mathbf{M} \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \frac{\mathbf{x}' \times \mathbf{p}_1}{|\mathbf{x}' - \mathbf{x}_R|^3} dV \right. \\ &\quad + \frac{\varepsilon_r - 1}{3} \varepsilon_0 \partial_t^2 \mathbf{M} \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \frac{\mathbf{x}' \times \mathbf{p}_1}{|\mathbf{x}' - \mathbf{x}_R|^3} dV \\ &\quad \left. + \varepsilon_0 \partial_t^2 \mathbf{M} \cdot \int_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} \frac{\mathbf{v} \times \mathbf{n}}{|\mathbf{x}' - \mathbf{x}_R|^2} dV \right] \end{aligned} \quad (48)$$

for $t > 0$ explicitly showing that time variations of the magnetization are received without any propagation delay in the quasi-static limit. We observe that, for magnetic field measurement, the conductivity and permittivity are present in the intermediate-field contribution to the signal ($1/\text{distance}^2$ term), while, for electric field measurement, the dielectric properties of the ball show up in the near field contribution to the signal ($1/\text{distance}^3$ term).

As we move away from the ball, the travel time τ will obviously increase. The above quasi-static signal models remain valid, however, provided that $|s|\tau \ll 1$ for all $\mathbf{x}' \in \mathbb{D}_{\text{obj}}$. It is obvious that the quasi-static signal models can no longer be used as soon as this inequality is not satisfied.

Finally, for later convenience, we write the quasi-static signals as

$$\begin{aligned} d_h^{QS}(t) &= \partial_t \mathbf{M} \cdot \mathbf{a}_1^h(\mathbf{x}_R) + \frac{\sigma \mu_0}{3} \partial_t^2 \mathbf{M} \cdot \mathbf{a}_2^h(\mathbf{x}_R) \\ &\quad + \frac{\varepsilon_r - 1}{3} \frac{1}{c_0^2} \partial_t^3 \mathbf{M} \cdot \mathbf{a}_2^h(\mathbf{x}_R) \text{ and} \end{aligned} \quad (49)$$

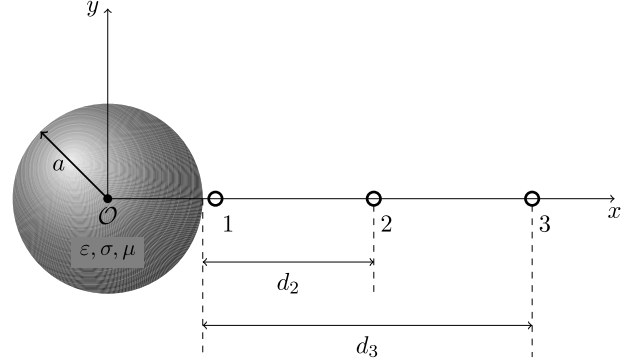


Fig. 1. FID signal measurement setup. A homogeneous ball with a radius a , centered at the origin has a permittivity ε , conductivity σ , and permeability μ . Relaxation times T_1 and T_2 .

TABLE I
DIELECTRIC MEDIUM PARAMETERS OF WHITE MATTER FOR DIFFERENT BACKGROUND FIELDS [19], [21]

B_0 [T]	1.5	3	7	11.2
f_L [MHz]	63.9	127.7	298	476.9
σ [S/m]	0.3	0.3	0.4	0.5
ε_r	68	53	44	41

$$\begin{aligned} d_e^{QS}(t) &= \frac{\sigma}{3} \partial_t \mathbf{M} \cdot \mathbf{a}_1^e(\mathbf{x}_R) + \frac{\varepsilon_r - 1}{3} \varepsilon_0 \partial_t^2 \mathbf{M} \cdot \mathbf{a}_1^e(\mathbf{x}_R) \\ &\quad + \varepsilon_0 \partial_t^2 \mathbf{M} \cdot \mathbf{a}_2^e(\mathbf{x}_R) \end{aligned} \quad (50)$$

where the expressions for the expansion vectors $\mathbf{a}_k^{\text{e,h}}(\mathbf{x}_R)$, $k = 1, 2$, are easily obtained from (47) and (48).

III. SIMULATIONS

To test the validity of our signal models and study the influence of the permittivity and conductivity of the ball on these signals, we consider the configuration illustrated in Fig. 1. In this configuration, all geometrical parameters are fixed and wavelength-independent since we want to investigate this setup in MR scanners with different background fields. In particular, the radius of the ball is set to $a = 2.5$ cm, and we use three receivers located on the x -axis to measure the various field responses. With Receiver 1 we carry out surface measurements, and in our simulations, this receiver is located at a distance $d_1 = 2.5 \cdot 10^{-6}$ cm from the ball. Receiver 2 is located at a distance of $d_2 = 25$ cm from the ball, and finally, Receiver 3 is located at a distance of $d_3 = 50$ cm from the ball. All three receivers are loops that have a circular surface area with a radius of 2 cm. This is the setup of our computer phantom, and all measurements described in this section are numerical simulations performed on this phantom. When we carry out a magnetic field measurement (emf), the loop is oriented in the x -direction ($\mathbf{v} = \mathbf{i}_x$), while, for an electric field measurement (mmf), we orient the loop in the z -direction ($\mathbf{v} = \mathbf{i}_z$). The signal models will be evaluated for background fields of 1.5, 3, 7, and 11.2 T. The resonance (and, therefore, measurement) frequency for each magnetic field strength is determined by the larmor precession frequency $f_L = \gamma B_0$, where $\gamma = 42.58$ MHz/T is the proton gyromagnetic ratio

and B_0 is the magnitude of the background field. The ball that we consider consists of white matter, and its conductivity and relative permittivity values at the Larmor frequencies that correspond to these background fields are listed in Table I. In all cases, the relative permeability is taken to be equal to one. For the relaxation times of white matter, we take those of a 3-T background field, $T_1 = 900$ ms, and $T_2 = 75$ ms [22], and we use these values for all background fields under consideration. More information on the dielectric properties of tissue can be found in [19] and [20], for example.

The signals that we receive are FID signals as generated by the time-varying magnetization

$$M_x(t) = M^{\text{eq}} e^{-t/T_2} \cos(\omega_0 t) \quad (51)$$

$$M_y(t) = -M^{\text{eq}} e^{-t/T_2} \sin(\omega_0 t) \quad (52)$$

$$\text{and } M_z(t) = M^{\text{eq}} (1 - e^{-t/T_1}) \quad (53)$$

where $\omega_0 = \gamma B_0$ is the Larmor frequency, T_1 and T_2 are the longitudinal and transverse relaxation times, respectively, and M^{eq} is the equilibrium magnetization. For a proton spin density $\rho = 6.69 \cdot 10^{28} \text{ m}^{-3}$ (water) and at $T = 310.15$ K, the equilibrium magnetization evaluates to $M^{\text{eq}} \approx 0.0031 B_0$. The above components of the magnetization form the solution of the Bloch equation with initial condition $\mathbf{M}(0) = M^{\text{eq}} \mathbf{i}_x$. For $t > 0$, the above solution describes how the magnetization relaxes back to its equilibrium $\mathbf{M} = M^{\text{eq}} \mathbf{i}_z$ as time increases.

A. Validating the Born Approximation

Before we carry out our signal analysis, we first validate the Born approximation for all background fields under consideration since our signal models are based on this approximation. Specifically, we compute the time-domain electromagnetic field due to the magnetization given by (51)–(53) using an in-house UPML-FDTD code. In our FDTD model, the conductivity and permittivity values of the ball at the various Larmor frequencies are selected according to Table I. Subsequently, we use the computed FDTD field responses and, subsequently, compute the electromotive force V_{emf} at the receiver location $\mathbf{x}_R = [3.2, 0, 0]$ cm. The dashed lines in Fig. 2 show the resulting signals for various background fields. The solid lines in this figure depict the signal model of (38) at the same receiver location and for the same background fields. This latter model is based on the quasi-static Born approximation (31) and (32), while obviously no such approximation has been applied in our FDTD simulations of our computer phantom. From Fig. 2, we observe that the signals based on FDTD modeling and the signals based on the quasi-static Born approximation overlap, thereby validating that for this configuration, and for all background fields of interest, the Born approximation, indeed, provides us with an accurate signal description.

B. Quasi-Static Signal Analysis

In the Laplace domain, the quasi-static signal models hold provided that the condition $|s|\tau \ll 1$ is satisfied for all $\mathbf{x}' \in \mathbb{D}_{\text{obj}}$ and all frequencies s of interest. For the FID signals as generated by the magnetization of (51)–(53), the Larmor

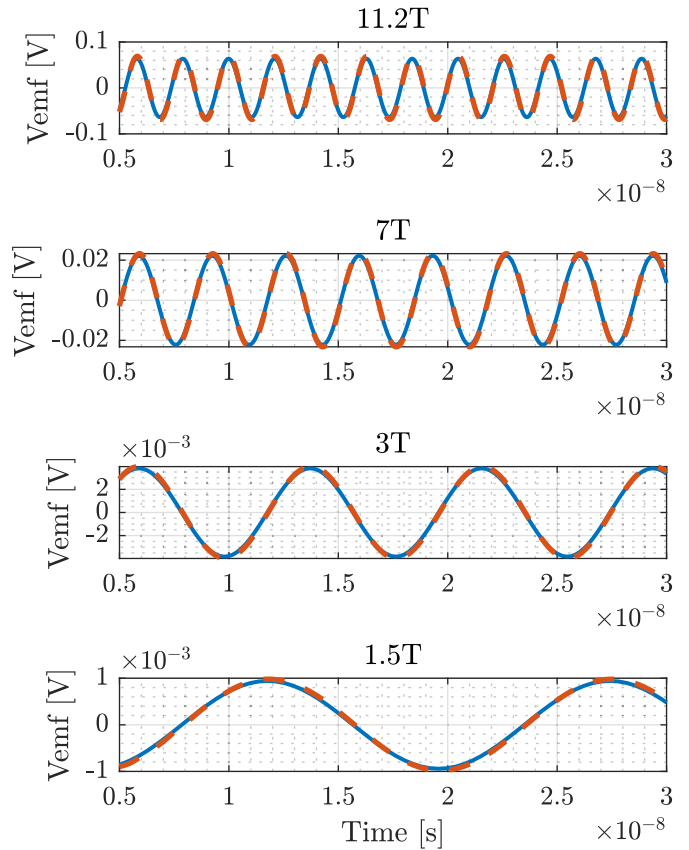


Fig. 2. Validation of the Born approximation for various background fields. Dashed (red) lines: V_{emf} as determined from the magnetic field of the FDTD simulation. Solid (blue) line: the signal model of (38). The receiver is located at $\mathbf{x}_R = [3.2, 0, 0]$ cm, and the medium parameters of the ball are listed in Table I.

frequency is the only nonvanishing oscillation frequency, and we can set $s = j\omega_0$ in the above condition to obtain the quasi-static requirement that $2\pi\lambda_0^{-1}|\mathbf{x}' - \mathbf{x}_R| \ll 1$ should hold for all $\mathbf{x}' \in \mathbb{D}_{\text{obj}}$, where λ_0 is the wavelength in free space. Introducing the maximum distance $d_{\text{max}} = \max_{\mathbf{x}' \in \mathbb{D}_{\text{obj}}} |\mathbf{x}' - \mathbf{x}_R|$, the quasi-static condition is satisfied if $2\pi d_{\text{max}}/\lambda_0 \ll 1$. Table II lists $2\pi d_{\text{max}}/\lambda_0$ for the three receivers mentioned above and for different background fields. From this table, we expect the quasi-static approximation to hold for Receiver 1 and essentially all background fields under consideration. For Receiver 2, the quasi-static signal models are expected to hold for 1.5 T and possibly 3 T background fields, while, for Receiver 3, the quasi-static field approximation possibly holds at 1.5 T only. Figs. 3–5 show the full-wave signal model of (38) (solid line) and the quasi-static signal model of (47) (dashed line) for the electromotive force V_{emf} at the three receivers of Fig. 1. Since a quasi-static electromotive or magnetomotive force signal analysis leads to the same conclusions, we present results for the electromotive force only.

From Figs. 3–5, we observe that the quasi-static parameters of Table II quite accurately predict when a quasi-static signal model can be used. Specifically, for Receiver 1, the value of $2\pi d_{\text{max}}/\lambda_0$ is at or below 0.5 for all background fields, and Fig. 3 shows that the full and quasi-static signals

TABLE II
BACKGROUND FIELDS AND NORMALIZED DISTANCES

B_0 [T]	1.5	3	7	11.2
λ_0 [m]	4.69	2.35	1.01	0.63
$2a/\lambda_0$	0.01	0.02	0.05	0.08
Rec. 1: $2\pi d_{\max}/\lambda_0$	0.07	0.13	0.31	0.5
Rec. 2: $2\pi d_{\max}/\lambda_0$	0.40	0.80	1.87	3.00
Rec. 3: $2\pi d_{\max}/\lambda_0$	0.74	1.47	3.44	5.50

essentially overlap. For Receiver 2, however, we observe that the quasi-static model overlaps with the full-wave model for a background field of 1.5 T but starts to deviate from the full-wave model for a background field of 3 T. For even higher background fields, the quasi-static model is no longer valid, which is consistent with Table II, since $2\pi d_{\max}/\lambda_0$ is larger than one in this case. These results indicate that the quasi-static signal model coincides with the full-wave model as long as $2\pi d_{\max}/\lambda_0 \leq 0.5$. This observation is consistent with the full-wave and quasi-static signal models for Receiver 3, as shown in Fig. 5. In this case, the quasi-static signal model already deviates from the full-wave model for a background field of 1.5 T for which we have $2\pi d_{\max}/\lambda_0 \approx 0.74$. For higher background fields, the quasi-static signal approximation definitely does not hold at Receiver 3, and we have to resort to the full-wave model of (47) in this case.

Finally, the dotted lines in Figs. 3–5 show the contribution of the conductivity and permittivity terms [the last two terms on the right-hand side of (47)] to the total quasi-static signal (47). We also observe that the contribution of these terms is small for lower background fields but increases as the background field strength increases. These simulation results indicate that the conductivity and permittivity of the ball can be retrieved from a quasi-static electromotive force measurement, provided that the SNR of the signals and the background field strengths are sufficiently large and the quasi-static field approximation holds. Another option is, of course, to use an electric field measurement (magnetomotive force measurement) as a basis for conductivity and permittivity retrieval since, for such a measurement, these quantities contribute to the signal via the near-field as opposed to an electromotive force measurement, where the medium parameters contribute to the signal via the intermediate field.

C. Conductivity and Permittivity Retrieval

Since the quasi-static signal models under the Born approximation are all valid for computer phantom measurements carried out with Receiver 1 and all background fields of interest, we now use these models at this receiver location to retrieve the conductivity and permittivity of the ball (white matter).

Let us start with the signal model for a magnetic field measurement given by (49). Introducing the functions $d_1^h(t) = \partial_t \mathbf{M} \cdot \mathbf{a}_1^h(\mathbf{x}_R)$, $d_2^h(t) = \mu_0 \partial_t^2 \mathbf{M} \cdot \mathbf{a}_2^h(\mathbf{x}_R)$, and $d_3^h(t) = c_0^{-2} \partial_t^3 \mathbf{M} \cdot$

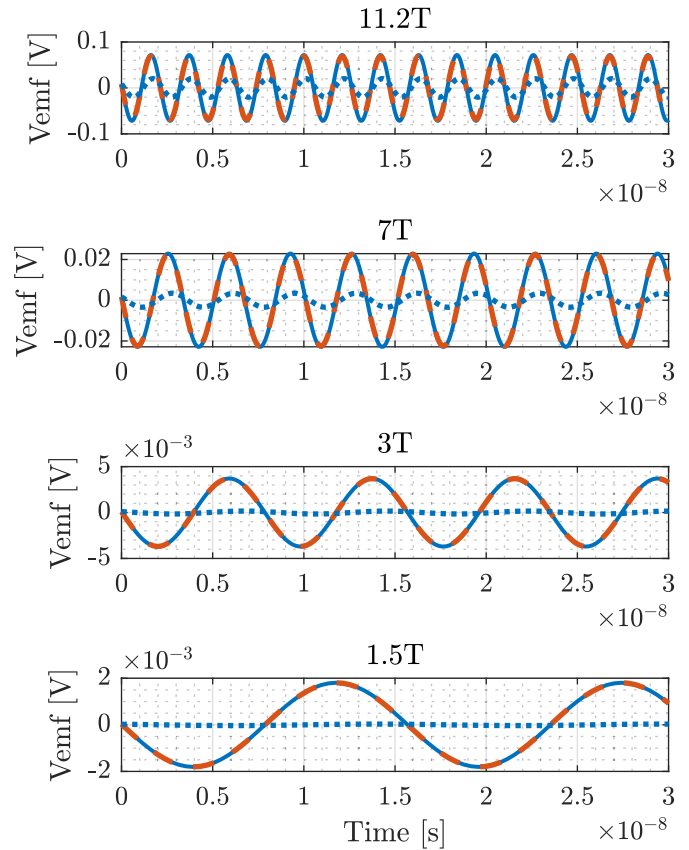


Fig. 3. Electromotive force at Receiver 1 for various background field strengths and a ball of white matter. The dielectric parameters are listed in Table I. Solid line: full-wave signal model of (38); dashed line: quasi-static signal model of (47); and dotted line: sum of the last two terms on the right-hand side of (47).

$\mathbf{a}_2^h(\mathbf{x}_R)$, we have

$$d_{h, \text{QS}}^{\text{Born}}(t) = d_1^h(t) + \frac{\sigma}{3} d_2^h(t) + \frac{\epsilon_r - 1}{3} d_3^h(t) \quad (54)$$

for $t > 0$. Similarly, for the electric field signal model, we have

$$d_{e, \text{QS}}^{\text{Born}}(t) = \frac{\sigma}{3} d_1^e(t) + \frac{\epsilon_r - 1}{3} d_2^e(t) + d_3^e(t) \quad (55)$$

for $t > 0$ with $d_1^e(t) = \partial_t \mathbf{M} \cdot \mathbf{a}_1^e(\mathbf{x}_R)$, $d_2^e(t) = \epsilon_0 \partial_t^2 \mathbf{M} \cdot \mathbf{a}_2^e(\mathbf{x}_R)$, and $d_3^e(t) = \epsilon_0 \partial_t^3 \mathbf{M} \cdot \mathbf{a}_3^e(\mathbf{x}_R)$.

Subsequently, we introduce the time instances $t_n = (n-1)\Delta t$ for $n = 1, 2, \dots, N$ with $(N-1)\Delta t = T_{\text{obs}}$, where T_{obs} is the length of the observation interval, and consider the above signals at these time instances to obtain

$$\mathbf{d}^h = \mathbf{d}_1^h + \frac{\sigma}{3} \mathbf{d}_2^h + \frac{\epsilon_r - 1}{3} \mathbf{d}_3^h \quad (56)$$

and

$$\mathbf{d}^e = \frac{\sigma}{3} \mathbf{d}_1^e + \frac{\epsilon_r - 1}{3} \mathbf{d}_2^e + \mathbf{d}_3^e \quad (57)$$

where $\mathbf{d}^h = [d_{h, \text{QS}}^{\text{Born}}(t_1), d_{h, \text{QS}}^{\text{Born}}(t_2), \dots, d_{h, \text{QS}}^{\text{Born}}(t_N)]^T$ is an N -by-1 column vector, and all other vectors in the above equation are defined similarly.

Since we consider FID signals as generated by the magnetization of (51)–(53), it immediately follows that the vector

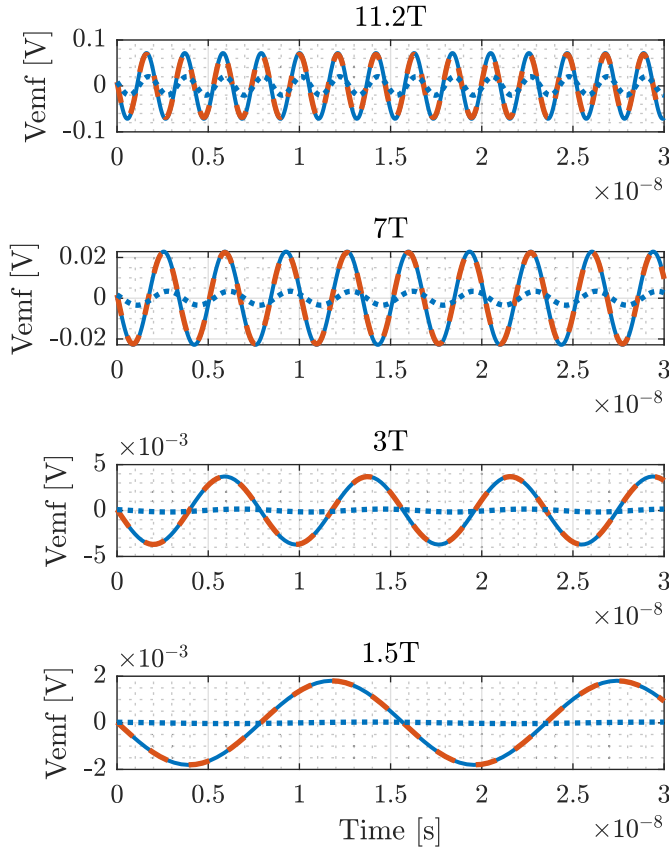


Fig. 4. Electromotive force at Receiver 2 for various background field strengths and a ball of white matter. The dielectric parameters are listed in Table I. Solid line: full-wave signal model of (38); dashed line: quasi-static signal model of (47); and dotted line: sum of the last two terms on the right-hand side of (47).

\mathbf{d}_1^h and \mathbf{d}_3^h and the vectors \mathbf{d}_2^e and \mathbf{d}_3^e are linearly dependent. Therefore, we consider the modified (scattered) data equations

$$\tilde{\mathbf{d}}^h = \mathbf{A}^h \mathbf{c} \quad \text{and} \quad \tilde{\mathbf{d}}^e = \mathbf{A}^e \mathbf{c} \quad (58)$$

with $\mathbf{c} = (1/3)[\sigma, \varepsilon_r - 1]^T$, $\tilde{\mathbf{d}}^h = \mathbf{d}^h - \mathbf{d}_1^h$, $\tilde{\mathbf{d}}^e = \mathbf{d}^e - \mathbf{d}_3^e$, and the matrices \mathbf{A}^h and \mathbf{A}^e have the column partitioning $\mathbf{A}^h = (\mathbf{d}_2^h, \mathbf{d}_3^h)$ and $\mathbf{A}^e = (\mathbf{d}_1^e, \mathbf{d}_2^e)$. Finally, noise is added to the data, and we attempt to reconstruct the medium parameters as

$$\mathbf{c}^* = \underset{\mathbf{c}}{\operatorname{argmin}} \|\tilde{\mathbf{d}}_n^{h,e} - \mathbf{A}^{h,e} \mathbf{c}\|_2^2 \quad (59)$$

where $\tilde{\mathbf{d}}_n^{h,e} = \tilde{\mathbf{d}}^{h,e} + \mathbf{n}$ is the noisy data vector with \mathbf{n} being the noise vector. With $T_0 = 2\pi/\omega_0$, we first take $T_{\text{obs}} = 3T_0 = O(10^{-8,9})$ s in our minimization problem. It is clear that the exponential decay of the FID signal can be neglected in this case. With an SNR of 20 dB, the conductivity and permittivity are determined by solving the corresponding least-squares problem (59), and the retrieved parameters are depicted in Fig. 6 along with the exact conductivity and permittivity values of white matter and for various background fields, as listed in Table I. From this figure, we observe that, for the magnetic field (emf) measurement model, the error in the retrieved medium parameters decreases as the background field strength increases. At 1.5 and 3 T, the medium parameters cannot be retrieved, but accurate medium parameters are obtained only

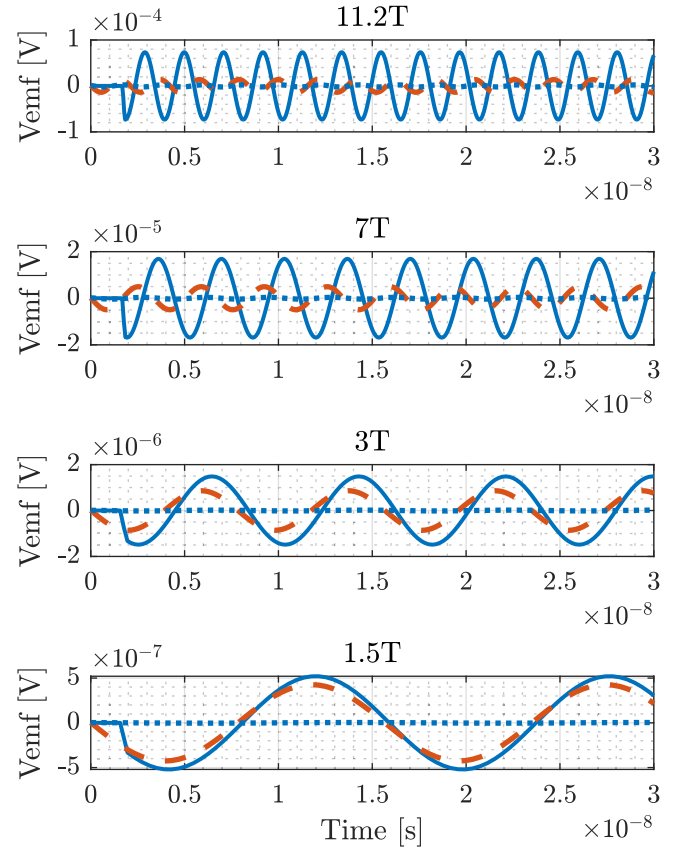


Fig. 5. Electromotive force at Receiver 3 for various background field strengths. The dielectric parameters are listed in Table I. Solid line: full-wave signal model of (38); dashed line: quasi-static signal model of (47); and dotted line: sum of the last two terms on the right-hand side of (47).

TABLE III
RECONSTRUCTION RESULTS FOR EMF AND MMF RECEIVERS,
AS DISPLAYED IN FIG. 6

B_0 [T]	1.50	3	7	11.20
σ^{True} [S/m]	0.30	0.30	0.40	0.50
$\hat{\sigma}^{\text{EMF}}$ [S/m]	0.26	0.41	0.37	0.50
$\text{err}^{\text{EMF}}[\%]$	12.80	40.94	8.05	0.18
$\hat{\sigma}^{\text{MMF}}$ [S/m]	0.30	0.30	0.40	0.50
$\text{err}^{\text{MMF}}[\%]$	1.40	0.43	0.98	0.32
$\varepsilon_r^{\text{True}}$	68	53	44	41
$\hat{\varepsilon}_r^{\text{EMF}}$	50.73	61.45	45.66	41.11
$\text{err}^{\text{EMF}}[\%]$	25.39	15.95	3.78	0.26
$\hat{\varepsilon}_r^{\text{MMF}}$	67.44	52.51	43.64	41.00
$\text{err}^{\text{MMF}}[\%]$	0.82	0.92	0.83	0.01

at 11.2 T. Since the dielectric medium parameters contribute via the near field to a signal that is based on an electric field (mmf) measurement, we expect that, when the electric field measurement model is used, these parameters can be reliably recovered for low and high background fields. From Fig. 6, we observe that this is, indeed, the case, and similar to the magnetic field measurement model, the reconstruction results improve as the strength of the background field increases. The reconstructed medium parameters at various background fields when electric and magnetic field measurement models are used

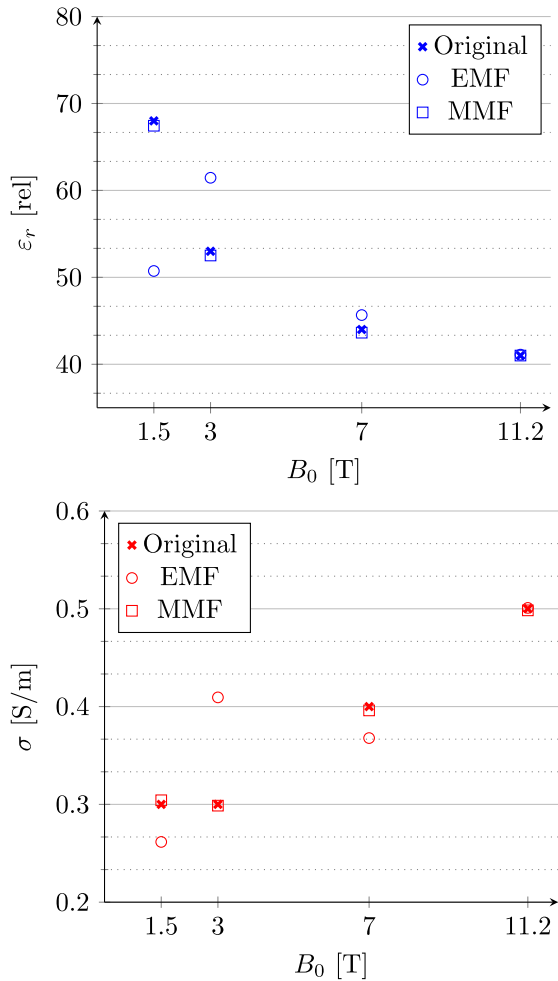


Fig. 6. Reconstructed permittivity (top) and conductivity (bottom) values using an EMF or MMF computer phantom measurement for various field strengths.

are summarized in Table III. Finally, we mention that we have repeated this experiment on an observation interval $T_{\text{obs}} = 3T_2 = O(10^{-2})$ s and found similar results, showing that the electrical properties can also be recovered on an $O(10^{-2})$ time scale.

IV. DISCUSSION AND CONCLUSION

In this article, we have presented full-wave signal models for MRI field measurements. The models show that the magnetization and the induced electric scattering currents contribute to the measured signals, both weighted by their respective receive fields that are determined by the antenna that is used for reception. We have shown that, to evaluate the models, Green's tensors of the background medium must be known, along with the dielectric properties of the object, and the magnetization within the excited part of the object must be known as well. For inhomogeneous background media, Green's tensors can only be evaluated numerically in general, which may be a formidable task especially if electrically large objects are of interest. Moreover, for given dielectric medium profiles and a given magnetization, the electric field strength within the object must be computed since it is required to determine the electric scattering source. In other words, apart from numeri-

cally computing Green's tensors of the background medium, a forward problem for the electric field strength must be solved as well. Despite these computational bottlenecks, direct evaluation is possible in principle. In addition, the models can be easily extended to include contrasts in permeability but at the expense of having to solve a coupled forward problem for the electric and magnetic field within the object of interest.

To obtain explicit closed-form signal representations for electric and magnetic field measurements, we have considered a homogeneous ball that is embedded in free space. It is obvious that Green's tensors of the background medium are now known, and if the dielectric parameters and radius of the ball are "sufficiently small," the quasi-static Born approximation applies meaning that the electric field within the ball may be approximated by the quasi-static background field, which is explicitly known. It is obvious that there is now no need to solve a forward problem, and the medium parameters show up explicitly in the resulting signal models. Travel time effects are still included in these models since the Born approximation applies to the electric field *within* the ball only. Quasi-static signal models may be obtained, however, for receiver locations for which travel time effects can be neglected. These signal models directly generalize the standard quasi-static models as normally used in MRI and clearly show how the dielectric parameters of the ball influence the measured signals. In fact, for FID signals obtained from an electric or magnetic field measurement, we demonstrated that the dependence of the signals on the medium parameters can even be used to retrieve these parameters. Specifically, using simulations, we showed that, for high background fields (7 and 11.2 T), electric (mmf) and magnetic (emf) field measurements allow for reliable parameter reconstructions, while, at lower field strengths, only electric field measurements can essentially be used because the dielectric parameters show up in the near-field of electric field measurement and not in the near-field of magnetic field measurement.

The simplified quasi-static models have their limitations, of course, and care should be taken when applying these models since they are valid for a ball and under very special circumstances only (quasi-static field and Born approximation apply). However, it is straightforward to construct a spherical phantom complying with these assumptions for a real-world experimental setup, and it is straightforward to measure the FID to validate this model, which the authors aim to do in future work.

It is obvious that the full-wave models do not suffer from these limitations and allow us to determine how inhomogeneous dielectric tissue profiles influence the measured signals. To validate the full-wave models, measurements of a more complex phantom can be used in much the same way as the validation of the simplified model. However, careful calibration of the phantom and measurement setup, and more complex full-wave simulations are necessary in this case. Large-scale computations are required to determine the effects of the conductivity and permittivity profiles on the measured signals, but the models can potentially be used in a wide variety of applications. For a known object and excitation profile, for example, the receive fields of the antennas can be

optimized for sensitivity to the electric properties or to avoid signal voids by minimizing interference effects. Optimizing for the local SAR that leads to tissue heating can also be performed by minimizing the electric field sensitivity for areas of high conductivity (since SAR is related to the product of these two quantities). In conclusion, complex wave propagation effects that take place within a body part of interest are captured by the signal models presented in this article, and the models allow for signal and antenna optimization in a variety of MR applications.

APPENDIX

EXPANSION VECTORS FOR TIME-DOMAIN SIGNAL MODELS

The expansion vectors in the vectorial sensitivity function \mathbf{S}^{mg} of (40) for a magnetic field measurement are given by

$$\mathbf{r}_0^{\text{mg}} = \mathbf{p}_1, \quad (60)$$

$$\mathbf{r}_1^{\text{mg}} = \mathbf{p}_1 + \frac{1}{3}Z_0\sigma[(\mathbf{x}' \cdot \mathbf{v})\mathbf{n} - (\mathbf{x}' \cdot \mathbf{n})\mathbf{v}] \quad (61)$$

$$\mathbf{r}_2^{\text{mg}} = \mathbf{p}_2 + \frac{1}{3}Z_0\sigma[(\mathbf{x}' \cdot \mathbf{v})\mathbf{n} - (\mathbf{x}' \cdot \mathbf{n})\mathbf{v}] + \frac{1}{3}(\varepsilon_r - 1)\frac{(\mathbf{x}' \cdot \mathbf{v})\mathbf{n} - (\mathbf{x}' \cdot \mathbf{n})\mathbf{v}}{|\mathbf{x}' - \mathbf{x}_R|} \quad (62)$$

$$\mathbf{r}_3^{\text{mg}} = \frac{1}{3}(\varepsilon_r - 1)\frac{(\mathbf{x}' \cdot \mathbf{v})\mathbf{n} - (\mathbf{x}' \cdot \mathbf{n})\mathbf{v}}{|\mathbf{x}' - \mathbf{x}_R|} \quad (63)$$

where Z_0 is the impedance of vacuum and ε_r is the relative permittivity of the ball. Furthermore, the expansion vectors in the vectorial sensitivity function \mathbf{S}^{el} of (41) for an electric field measurement are given by

$$\mathbf{r}_0^{\text{el}} = \frac{\sigma}{3}\mathbf{x}' \times \mathbf{p}_1, \quad (64)$$

$$\mathbf{r}_1^{\text{el}} = Y_0\mathbf{q} + \frac{\sigma}{3}\mathbf{x}' \times \mathbf{p}_1, \quad (65)$$

$$\mathbf{r}_2^{\text{el}} = Y_0\mathbf{q} + \frac{\sigma}{3}\mathbf{x}' \times \mathbf{p}_2, \quad (66)$$

$$\mathbf{r}_3^{\text{el}} = \frac{1}{3}Y_0(\varepsilon_r - 1)\frac{\mathbf{x}' \times \mathbf{p}_2}{|\mathbf{x}' - \mathbf{x}_R|} \quad (67)$$

where $Y_0 = (\varepsilon_0/\mu_0)^{1/2}$ is the admittance of vacuum, and

$$\mathbf{q} = \mathbf{v} \times \mathbf{n} + \frac{1}{3}(\varepsilon_r - 1)\frac{\mathbf{x}' \times \mathbf{p}_1}{|\mathbf{x}' - \mathbf{x}_R|}. \quad (68)$$

Note that these expansion vectors are independent of s but do depend on the distance $|\mathbf{x}' - \mathbf{x}_R|$.

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