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Synthetic life on a chip

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Abstract

In this perspective, we argue that on-chip microfluidic systems provide an attractive technology when it comes to designing synthetic cells. We emphasize the importance of the surrounding environment for both living systems in nature and for developing artificial self-sustaining entities. On-chip microfluidic devices provide a high degree of control over the production of cell-like synthetic entities as well as over the local microenvironment that these soft-matter-based synthetic cells experience. Rapid progress in microfluidic fabrication technology has led to a variety of production and manipulation tools that establish on-chip environments as a versatile platform and arguably the best route forward for realizing synthetic life.

Keywords: synthetic cells; microfluidics; lab-on-a-chip devices; liposomes; coacervates

The curious thing called life

Some of the most intriguing questions that scientists – and laymen for that matter – ask, revolve around the theme of ‘What is life?’. For example, ‘What distinguishes living systems from lifeless matter’, ‘By what criteria can an entity be called alive?’, ‘Can we build life from scratch?’, ‘What minimal elements are needed to constitute a living cell?’. While scientists have been struggling to answer these questions for over at least a century, the emerging field of synthetic biology may now provide new avenues to shed some light on this. Indeed, efforts are springing up to attempt to assemble a cell-like object from lifeless molecular components in such a way that it will exhibit many of the attributes of living cells – in other words, to manufacture a synthetic cell that is alive^{1,2}. This is expected to lead to vast new insights into the cell biology and create new opportunities in biotechnology, while such research may also be highly relevant for astrobiology and how life began in the first place on our primitive earth. The field aimed at resolving the origin of life is facing enigmatic problems as it is very hard to get a hang of how millions of biomolecules self-organize to form autonomous self-sustaining systems. Systematically working on simplified minimal systems may help disentangling some of the enormous complexity. While embarking on the monumental task of revealing the basic principles of life with a synthetic-cell approach, it is useful to ask whether there are general lessons to consider from observing the current life forms in nature and what specific technologies are available that might facilitate the way.

The role of the external environment

Upon looking at the remarkable variety of life forms that exist on earth, one thing is immediately noticeable: the local environment plays a critical role for the survival of a particular life form. To survive and proliferate, we humans, for example, require quite specific conditions such as a certain range of external temperature, oxygen content of the air, water and food supplies, a symbiosis with our microbiota, etc. Changes in these conditions can be tolerated to some extent, but drastic changes, say a

temperature shift to ± 100 °C, would make human life unsustainable. The defined nature of the environment is thus crucial to our existence. This general point becomes even clearer when you consider the life of an obligatory parasite, an organism that cannot sustain itself without another host organism that provides it with indispensable nutrients. For example, *Nerocila* ectoparasites attach themselves to a host fish and entirely depends on the host for survival³. While without doubt *Nerocila* is alive, it would not be able to survive without the extremely specific environment of its host which provides it with essential components. An example at the unicellular level is *Mycoplasma genitalium*, a pathogenic bacterium that lives within the urinary tracts of humans (Fig.1a). The environment of the post-kidney urinary tracts is well-defined and has allowed *M. genitalium* to evolve to a rather minimal cellular organism with one of the smallest known genomes⁴, where many of the cellular networks were dropped that similar bacterial systems possess to robustly survive in more demanding conditions. Indeed, it is no surprise that the *Mycoplasma* species were selected by Venter and co-workers as the organisms of choice in The Minimal Genome Project, a study to find the smallest set of genetic material necessary to sustain life⁵.

Thus, life benefits from a specific external environment, a fact that generally is taken rather for granted. If the environment is rich and well-defined over a long time, the living form can be simplified in terms of the functions that it needs to perform. If, on the other hand, the environment is poor and strongly fluctuating, organisms need a robust array of functionalities to survive. Defining life for an object thus involves a subtle balance between the control and complexity that is provided by the environment against the built-in functions of the organism itself (Fig. 1b). It is interesting to consider whether we can extend this concept and take advantage of this in our pursuit of creating synthetic cells where we aim to mimic basic life-like characteristics, say a growth-replication-division cycle, in a population of microcontainers. For example, we may try to provide a very specific and rich environment in an attempt to make a synthetic cell that is as minimal possible with regards to its internal complexity and functionality. But how can one

spatiotemporally regulate and control the external environment while observing the microscopic synthetic cells? On-chip microfluidic technology provides an exquisite solution for this.

Microfluidics: an optimal way to control the environment

Microfluidic systems constitute a technology developed to handling small fluid volumes (in the μL range or less) flowing at the micrometer scale (typically with velocities of $\mu\text{L}/\text{min}$ or less). A microfluidic architecture typically comprises of a network of microchannels, ranging from sub-100 nm to hundreds of μm in diameter, that are mutually connected in a user-defined manner, through which fluids of specified composition can be flown with a high degree of control (Fig. 2a). A wide range of valves, splitters, mixers, gates, traps, and other local manipulation tools have been developed to manipulate the flow of fluids, particles, and cells on chip. Highly sophisticated and intricate microfluidic circuits can be designed to create user-specific microenvironments in a high-throughput fashion⁶ (Fig. 2b). Continuous development in microfluidics, coupled with advances in materials and fabrication, has opened up a tremendous potential to form complex multifunctional microfluidic systems that can handle thousands of cells in parallel, which can be particularly useful in the field of biomedicine and bioengineering⁷. In the light of the ideas sketched above regarding organism-environment relations, it is clear that microfluidics can provide unprecedented control over the environment and manipulation of synthetic cells, especially in comparison with traditional bulk experiments (the likes of pipetting fluids in Eppendorf tubes). Indeed, over the years, microfluidic schemes have been developed for a variety of on-chip production methods to make cell-like microcontainers that can potentially act as a scaffold to create synthetic cells, as well as manipulation tools to position, control, and maneuver such soft-matter-based micron-sized objects^{8,9}. Below, we briefly discuss these two points.

Producing synthetic cells on-chip

Pioneering work by the Weitz lab, who produced water-in-oil-in-water double-emulsion droplets using glass capillary devices in a process akin to bubble-blowing (Fig. 2c), set the tone of using microfluidics to create cell-like containers¹⁰. These micron-sized droplets with ideal encapsulation properties can be formed in a highly controlled and a high-throughput fashion, with follow-up work enabling the formation of compartmentalized multi-component droplets¹¹ (Fig. 2d-e). Recently, this droplet-based approach was redesigned to form liposomes (bilayer-bounded aqueous compartments in an aqueous external environment). Having a lipid bilayer as the boundary, such liposomes are close mimics of natural cells and thus more relevant for functional synthetic cell containers. The two prominent methods that utilize this approach are PDMS (polydimethylsiloxane)-based Octanol-assisted Liposome Assembly (OLA)¹² (Fig. 2f-h) and glass-capillary-based double emulsion-dewetting¹³. In both cases, the organic solvent phase physically separates within a few minutes to form unilamellar liposomes with a high encapsulation efficiency. Several other methods have emerged to form liposomes on chip¹⁴, and new techniques are continuously being developed (Fig. 2i-k), such as recently developed droplet-stabilized liposome production¹⁵. In parallel, these on-chip techniques are being utilized to make other promising scaffolds for building a synthetic cell¹⁶, such as polymersomes^{17,18} (using amphiphilic block copolymers) and proteinosomes¹⁹ (using protein-polymer conjugates). The on-chip approach further allows the formation of sophisticated and biologically relevant nested assemblies, such as liposome-in-liposome structures²⁰, also known as vesosomes, resembling eukaryotic cells with membrane-bound organelles such as the nucleus (Fig. 2l).

The microfluidic approach is also being extended into the domain of biomolecular condensates, membraneless organelles that are crucial to maintain the cellular biochemistry²¹. Usually formed through the process of complex coacervation, the bulk coacervate phase can be broken down by hydrodynamic focusing into relatively monodisperse droplets²² (Fig. 2m-o). Combining the two containers, coacervate-

in-liposome structures have been recently designed, either by encapsulating both the necessary components and modulating the phase transition parameter such as temperature²³ or by administering a coacervate component across the membrane through membrane-embedded protein pores²⁴ (Fig. 2p). The rapid development of various on-chip techniques is thus allowing a wide choice of methods to create cell-like containers as per the experimental need. The impressive level of control and sophistication provided by microfluidics is very difficult to achieve in bulk experimentation. Apart from the ability to synthesize objects in a highly controlled and a high-throughput fashion, the on-chip approach simultaneously gives the opportunity to store and to protect these soft-matter-based objects by providing a suitable microenvironment for storage, manipulation, and readout.

Manipulating synthetic cells on-chip

A major advantage of microfluidics is that synthetic cells, once produced on chip, can be further manipulated in a variety of useful ways, via numerous specific modules²⁵. The past years have seen the development of many features that could be useful for functionalizing minimal cells:

(i) Trapping: Keeping the synthetic cells in a fixed position is beneficial if one wants to modulate the external buffer conditions and study the cellular response. As a simple solution, objects can be immobilized in physical traps and monitored for hours²⁶ (Fig. 3a). This enables long-term observation and facilitates changing the external conditions without disturbance. Interestingly, the trap geometries can also be chosen such that they deform the containers into desired shapes²⁷, for example, a rod shape resembling the *E. coli* bacterium (Fig. 3b).

(ii) Controlling the external environment: Once immobilized or confined within a region, monitoring the environment becomes an easy task, for example, through feeding channels and switchable valves²⁸. One particularly useful feature is a dial-a-wave junction, where fluids from two input channels can be mixed in the desired ratio over a wide range (continuously from 100% of input 1 (and 0% of input 2) to 0% of input

1 (and 100% of input 2), Fig. 3c)²⁹. Combining this module with trap arrays facilitates to easily change the local environment in a user-defined manner.

(iii) Sorting: For large populations of vesicles, sorting modules are useful when it comes to selecting a specific fraction of vesicles, for example in experiments on directed evolution. Such sorting of droplets has been successfully demonstrated using dielectrophoresis, where in-built electrodes are able to sort water-in-oil droplets in a high-throughput manner³⁰ (Fig. 3d). Importantly, such sorting can be coupled with fluorescence-detection³¹, similar to fluorescence-activated cell sorting.

(iv) Local injection: Adding components in a defined manner to an existing object is very handy, especially when one wants to activate reactions in a particular sequence or achieve a step-by-step bottom-up assembly¹⁵. Electromicrofluidics has been shown to be capable of sequentially injecting picolitre fluid volumes into pre-formed droplets³² (Fig. 3e).

(v) Multiplication and division: Division is a fundamental requisite for life, needed for achieving perpetuation. Using straightforward triangular PDMS-based splitter posts, double-emulsion droplets and even liposomes can be divided efficiently (Fig. 3f-g)^{33,34}. Putting such splitters in series can lead to substantial amplification of the number of droplets³³ (Fig. 3f).

(vi) Growth: Growth is another fundamental characteristic of living systems that also will be a mandatory feature of synthetic cells. Recent work has demonstrated membrane tension-mediated growth of liposomes by trapping the liposomes and inducing membrane fusion with feeder liposomes present in the external bath³⁵ (Fig. 3h).

(vii) Compartmentalization of reactions: Microfluidic fabrication schemes enable the formation of sophisticated structures, which also provides a direct solution for segregating various biochemical reactions, something living cells have developed over the course of evolution. For example, coacervate-in-liposome structures can be used to carry out enzymatic reactions specifically within the condensates²⁴

(Fig. i). Vesosomes can be used to mimic the eukaryotic cell structure and limit *in vitro* transcription to the nucleus-mimicking liposome²⁰ (Fig. j).

Outlook: Towards synthetic life on chip

We started this perspective by emphasizing the importance of the external environment when it comes to the emergence and sustenance of living systems. One should rather not think of defining a living entity as an individual system in isolation, because its maintenance is inevitably connected to its habitat. Depending on the complexity and richness of the habitat, a living form can be a relatively simple system, as is exemplified with the case of parasitic pathogens. We argue that the same logic can beneficially be applied to synthetic life forms: one should be able to design minimal artificial cells by incubating them in a highly sophisticated micro-environment that will be responsible for their nourishment. An outstanding technology that provides such a well-defined dynamic environment is microfluidics. From the brief expose given above, it may be clear that microfluidics has truly changed the experimental approach, providing ample options for novel designs when it comes to creating and functionalizing synthetic cells. The high degree of control achieved with on-chip systems in creating, sustaining, and manipulating synthetic cells is next to none, and can be expected to play a vital role in the future of synthetic biology. Though the spatial constraints may be different, as a chip is a more specific environment than the natural one, we expect that future life-on-a-chip will essentially not be too much different from the natural life as we know it: functional, autonomous, and self-propagating units that are able to work within a particular set of conditions.

Summary Points

- The external environment is essential to a living system and determines how complex a natural/synthetic cell needs to be in order to sustain and perpetuate itself.

- When it comes to creating synthetic cells, it is beneficial to start with designing a very rich environment, in order to minimize the complexity of the synthetic cells.
- On-chip microfluidic techniques provide a versatile toolbox to produce synthetic cells in a controlled manner and to manipulate the cells as well as the external environment, and hence can be expected to significantly impact the future creation of synthetic life.

Conflict of interest

The authors declare no conflict of interest.

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Author contribution

S.D. and C.D. wrote the manuscript.

References

1. Szostak, J. W., Bartel, D. P. & Luisi, P. L. Synthesizing life. *Nature* **409**, 387–390 (2001).
2. <http://www.syntheticcell.eu>.
3. Nagler, C. & Haug, J. T. Functional morphology of parasitic isopods: understanding morphological adaptations of attachment and feeding structures in *Nerocila* as a pre-requisite for reconstructing the evolution of Cymothoidae. *PeerJ* **4**, e2188 (2016).
4. Fraser, C. M. *et al.* The minimal gene complement of *Mycoplasma genitalium*. *Science* **270**, 397–403 (1995).
5. Hutchison, C. A. *et al.* Design and synthesis of a minimal bacterial genome. *Science* **351**, aad6253–aad6253 (2016).
6. Thorsen, T., Maerkl, S. J. & Quake, S. R. Microfluidic large-scale integration. *Science* (2002). doi:10.1126/science.1076996
7. Hou, X. *et al.* Interplay between materials and microfluidics. *Nat. Rev. Mater.* **2**, (2017).
8. Shang, L., Cheng, Y. & Zhao, Y. Emerging Droplet Microfluidics. *Chem. Rev.* **117**, 7964–8040 (2017).
9. Martino, C. & DeMello, A. J. Droplet-based microfluidics for artificial cell generation: A brief review. *Interface Focus* **6**, (2016).
10. Zingsheim, H. P. *et al.* Monodisperse double emulsions generated from a microcapillary device. *Science* **308**, 537–541 (2005).
11. Adams, L. L. A. *et al.* Single step emulsification for the generation of multi-component double emulsions. *Soft Matter* **8**, 10719–10724 (2012).
12. Deshpande, S., Caspi, Y., Meijering, A. E. C. & Dekker, C. Octanol-assisted liposome assembly on chip. *Nat. Commun.* **7**, 10447 (2016).
13. Deng, N. N., Yelleswarapu, M. & Huck, W. T. S. Monodisperse Uni- and Multicompartment

- Liposomes. *J. Am. Chem. Soc.* **138**, 7584–7591 (2016).
14. Van Swaay, D. & Demello, A. Microfluidic methods for forming liposomes. *Lab on a Chip* **13**, 752–767 (2013).
 15. Weiss, M. *et al.* Sequential bottom-up assembly of mechanically stabilized synthetic cells by microfluidics. *Nat. Mater.* **17**, 89–95 (2018).
 16. Spoelstra, W. K., Deshpande, S. & Dekker, C. Tailoring the appearance: what will synthetic cells look like? *Current Opinion in Biotechnology* **51**, 47–56 (2018).
 17. Petit, J., Polenz, I., Baret, J. C., Herminghaus, S. & Bäumchen, O. Vesicles-on-a-chip: A universal microfluidic platform for the assembly of liposomes and polymersomes. *Eur. Phys. J. E* **39**, (2016).
 18. Shum, H. C., Kim, J. & Weitz, D. A. Microfluidic Fabrication of Monodisperse Biocompatible and Biodegradable Polymersomes with Controlled Permeability. *J. Am. Chem. Soc.* **130**, 9543–9549 (2008).
 19. Ugrinic, M. *et al.* Microfluidic formation of proteinosomes. *Chem. Commun.* **54**, 287–290 (2018).
 20. Deng, N., Yelleswarapu, M., Zheng, L. & Huck, W. T. S. Microfluidic Assembly of Monodisperse Vesosomes as Artificial Cell Models. *J. Am. Chem. Soc.* **139**, 587–590 (2017).
 21. Shin, Y. & Brangwynne, C. P. Liquid phase condensation in cell physiology and disease. *Science* **357**, eaaf4382 (2017).
 22. Vanswaay, D., Tang, T. Y. D., Mann, S. & DeMello, A. Microfluidic Formation of Membrane-Free Aqueous Coacervate Droplets in Water. *Angew. Chemie - Int. Ed.* **54**, 8398–8401 (2015).
 23. Deng, N.-N. & Huck, W. T. S. Microfluidic Formation of Monodisperse Coacervate Organelles in Liposomes. *Angew. Chemie - Int. Ed.* **56**, 1–6 (2017).
 24. Deshpande, S. *et al.* Spatiotemporal control of coacervate formation within liposomes. *Nat. Commun.* **10**, 1800 (2019).
 25. Göpflich, K., Platzman, I. & Spatz, J. P. Mastering Complexity: Towards Bottom-up Construction of

- Multifunctional Eukaryotic Synthetic Cells. *Trends Biotechnol.* **xx**, 1–14 (2018).
26. Nahas, K. Al *et al.* A microfluidic platform for the characterisation of membrane active antimicrobials. *Lab Chip* (2018).
 27. Fanalista, F. *et al.* Shape and Size Control of Artificial Cells for Bottom-Up Biology. *ACS Nano* (2019). doi:10.1021/acsnano.9b00220
 28. Beebe, D. J., Mensing, G. A. & Walker, G. M. Physics and Applications of Microfluidics in Biology. *Annu. Rev. Biomed. Eng.* **4**, 261–286 (2002).
 29. Kaiser, M. *et al.* Monitoring single-cell gene regulation under dynamically controllable conditions with integrated microfluidics and software. *Nat. Commun.* (2018). doi:10.1038/s41467-017-02505-0
 30. Ahn, K. *et al.* Dielectrophoretic manipulation of drops for high-speed microfluidic sorting devices. *Appl. Phys. Lett.* **88**, 024104 (2006).
 31. Baret, J. C. *et al.* Fluorescence-activated droplet sorting (FADS): Efficient microfluidic cell sorting based on enzymatic activity. *Lab Chip* **9**, 1850–1858 (2009).
 32. Abate, A. R., Hung, T., Mary, P., Agresti, J. J. & Weitz, D. A. High-throughput injection with microfluidics using picoinjectors. *Proc. Natl. Acad. Sci.* **107**, 19163–19166 (2010).
 33. Abate, A. R. & Weitz, D. a. Faster multiple emulsification with drop splitting. *Lab Chip* **11**, 1911–1915 (2011).
 34. Deshpande, S., Spoelstra, W. K., Van Doorn, M., Kersemakers, J. & Dekker, C. Mechanical Division of Cell-Sized Liposomes. *ACS Nano* **12**, 2560–2568 (2018).
 35. Deshpande, S., Wunnava, S., Hueting, D. & Dekker, C. Membrane tension-mediated growth of liposomes. *Under Revision in Small*
 36. Deshpande, S. & Dekker, C. On-chip microfluidic production of cell-sized liposomes. *Nat. Protoc.* (2018). doi:10.1038/nprot.2017.160

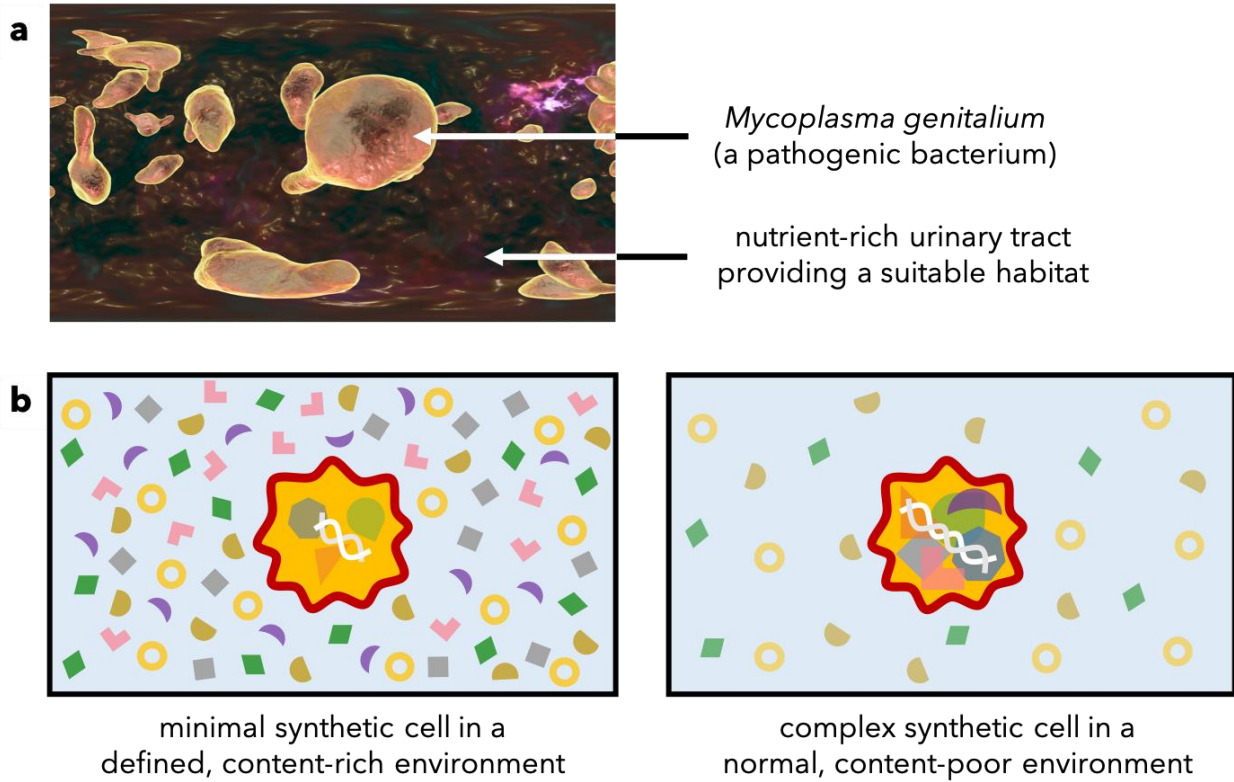


Figure 1: The importance of a suitable environment to sustain life.

(a) Artist impression of the pathogenic bacterium *Mycoplasma genitalium* that inhabits the urinary tract of humans, which provides it with a nourishing environment. (b) The complexity of a living form, or of a synthetic cell for that matter, depends on the surrounding environment. If the environment is a rich medium that provides the cell with a large variety of nutrients and other essential molecules, synthetic cell may be relatively minimalistic (left). Making the environment less specific does necessitate the increase the complexity of the internal machineries of the synthetic cell (right).

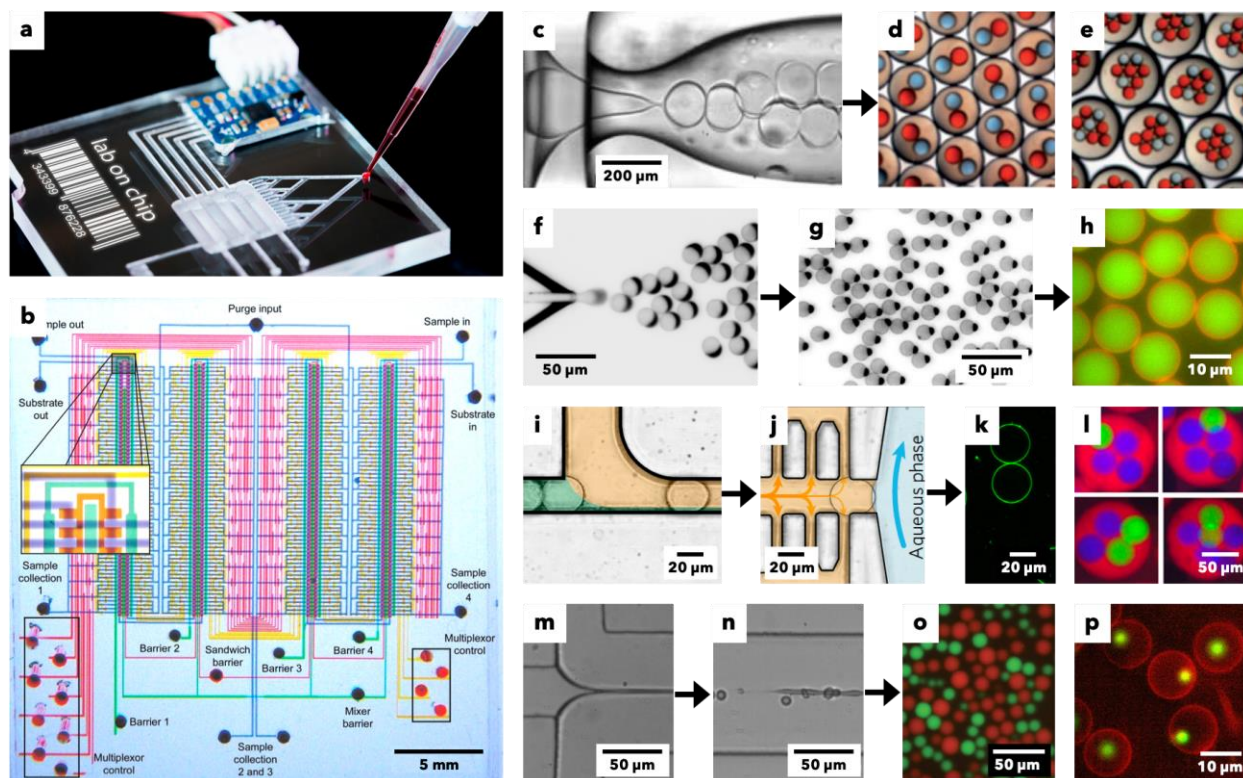


Figure 2: The large variety of on-chip technologies available to produce synthetic cells.

(a) Example of a lab-on-a-chip device that shows its miniature size, microchannel architecture capable of handling minute fluid samples, and its ability to couple with diverse modules such as electronics. (b) Large-scale integrated microfluidic circuit containing an intricate network of thousands of channels, valves, and chambers, demonstrating the capability of a microfluidic chip to create and control a complex environmental set-up. (c-e) High-throughput production of monodisperse double-emulsion droplets using glass-capillary devices (c). These glass-capillary devices can be further designed to allow sub-compartmentalization (red and blue inner drops), exemplified by two (d) and eight (e) inner drops inside the main droplet. (f-h) Octanol-assisted Liposome Assembly (OLA) showing the initial formation of double-emulsion droplets at the production junction (f), partially dewetted liposomes with protruding octanol pockets (g), and completely dewetted monodisperse liposomes (h). (i-k) Droplet-stabilized liposome formation, where the polymer-coating on the droplets is first destabilized at the T-junction by the oil phase (in yellow) containing surfactants (i) and droplets are eventually released into the aqueous phase

(j), forming unilamellar liposomes (k). **(l)** Vesosomes (liposomes-in-liposome structures) with different numbers and ratios of interior liposomes (green and blue circles), formed using glass-capillary devices. **(m-o)** Microfluidic formation of coacervates, where the bulk coacervate phase is hydrodynamically focused (m) and pinched off to form irregular segments (n), which eventually form stable coacervate droplets (o). **(p)** Coacervate-in-liposome structures showing freely-diffusing polylysine/ATP coacervates (green blobs) formed inside OLA-based liposomes. Panels are adapted from references as follows: b: ⁶, c: ¹⁰; d-e: ¹¹; f-g: ³⁶; h: Cees Dekker lab; i-k: ¹⁵; l: ²⁰; m-o: ²²; p: ²⁴.

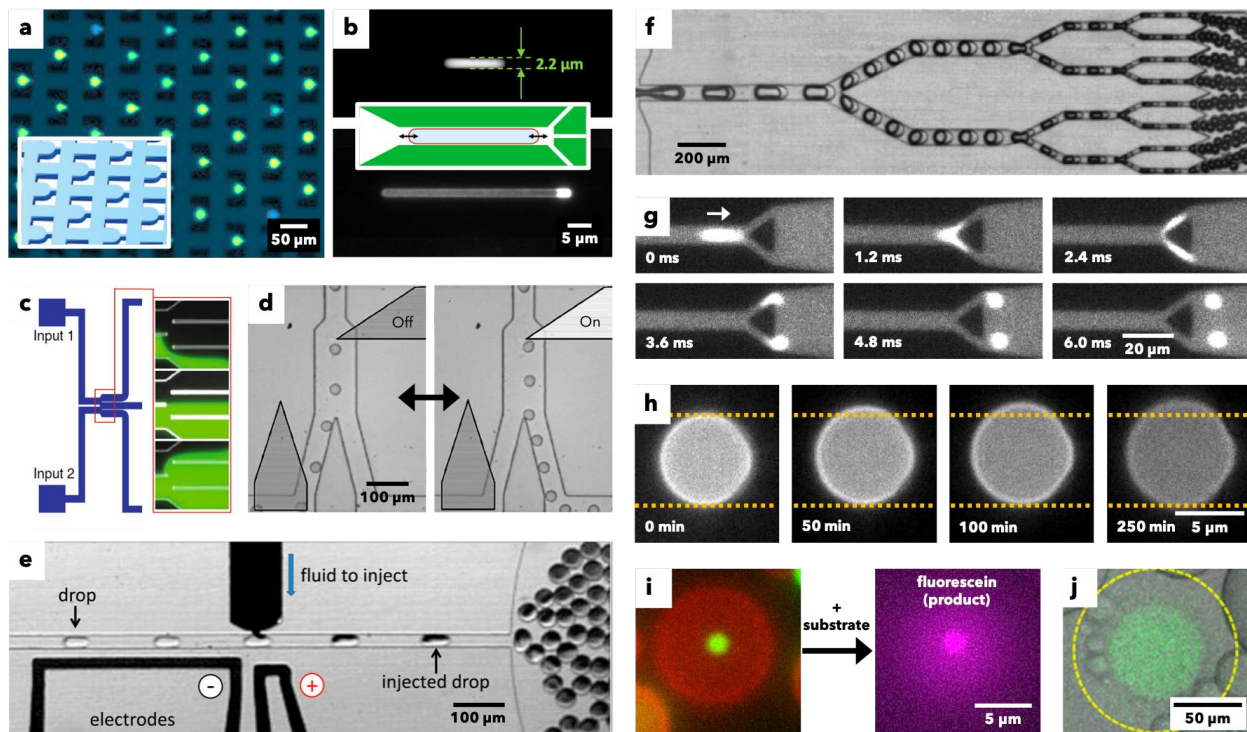


Figure 3: Variety of on-chip modules available to manipulate synthetic cells. (a-b) Trapping: An array of physical traps (design shown in the inset) showing highly efficient immobilization of liposomes on chip (a). Tubular trap design (inset in b) to deform synthetic cells into a specific shape, for example into rod-shaped geometry of different dimensions. The trapped objects are droplets (upper image in b) and double-emulsion droplets (lower image in b). (c) Controlling the external environment: Dial-a-wave junction with three distinct switching states (100% from input1, 50% each from input 1 and 2, 100% from input 2). This module can be combined with, for example, physical traps to change the local environment of the synthetic cells in a user-defined manner. (d) Sorting: a dielectrophoresis-based high-speed sorting of droplets. In absence of electric field, the droplets flow into the low-resistance channel (left panel), while, upon applying the electric field, they are attracted towards the energized electrode and enter the other channel. (e) Local injection: An on-chip picoinjector injects a well-defined amount of fluid into pre-formed droplets. The process is triggered by electric field, which is applied by the in-built electrodes. (f-g) Multiplication and division: Double-emulsion droplets splitting three times in series, resulting in eight-fold

amplification (f). Highly symmetric and leakage-free division of a cell-sized liposome across a mechanical splitter. The arrow indicates the direction of motion (g). (h) Growth: Time-lapse images showing membrane tension-mediated growth of a trapped liposome. A solution containing small feeder liposomes, which fuse with the trapped liposome, is continuously flushed resulting in the observed growth. The dashed horizontal lines are drawn in order to guide the eye. (i-j) Compartmentalized reactions: A coacervate-in-liposome structure (left panel in i) showing an enzymatic reaction predominantly getting carried out in the coacervate phase as judged by the fluorescence intensity of the resulting product (right panel in i). *In vitro* transcription being carried out specifically in the nucleus-mimicking liposome of a vesosome, as judged from the fluorescence (j). The yellow circle indicates the outer liposome boundary. Panels are adapted from references as follows:- a: ²⁶; b: ²⁷, c: ²⁹; d: ³⁰, e: ³²; f: ³³; g: ³⁴, h: ³⁵, i: ²⁴; j: ²⁰.